# Assessment of connectivity with MEG

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# Outline

- Crash course on source modelling
- MEG Source estimation in the HCP
- Estimation of connectivity from sourcereconstructed MEG data
- Connectivity estimation using spectrally resolved connectivity metrics
- MEG Connectivity estimation in the HCP
- Some notes on parcellations

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# What produces the electric current and magnetic field



#### Equivalent current dipoles



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#### Note: dipole moment is a vectorial quantity

forward model



forward model



forward model



- Volume conduction model of the head needed to model the volume currents associated the primary neuronal currents
- Cortical sheet based source model (8004 vertices) defines the locations at which the activity is going to be estimated
- Coregistration information needed to tie everything together in space

- Volume conduction model of the head needed to model the volume currents associated the primary neuronal currents
- Mesh describing the inner surface of the skull

- Cortical sheet based source model (8004 vertices) defines the locations at which the activity is going to be estimated
- Based on the surface-registered 32k midthickness meshes

- Coregistration information needed to tie everything together in space
- Necessary evil due to different conventions in coordinate systems
- MEG employs external landmarks-based ALS
- MRI employs brain anatomy based RAS
- ASCII text file with 4x4 Affine matrices

forward model

$$X = I_1 s_1 + I_2 s_2 + ... + I_n s_n + noise$$

forward model

$$X = I_1 s_1 + I_2 s_2 + \dots + I_n s_n + noise$$
  
X = LS + noise

forward model



#### Leadfields represent 'spatial fingerprints'



forward model

$$X = I_1 s_1 + I_2 s_2 + \dots + I_n s_n + noise$$
  
X = LS + noise

$$\hat{S} = W^T X$$

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# MEG source estimation in the HCP

- Beamforming: scan a set of pre-specified dipole locations, and create a spatial filter with: w<sup>T</sup>=(I<sup>T</sup>C<sup>-1</sup>I)<sup>-1</sup>I<sup>T</sup>C<sup>-1</sup>
- Distributed source modelling with a weighted minimum norm constraint: W<sup>T</sup>=RL<sup>T</sup>(LRL<sup>T</sup>+λN)<sup>-1</sup>

# MEG source estimation in the HCP

- Beamforming: tMEG data + rMEG data
- Distributed source modelling with a weighted minimum norm constraint: rMEG data

## MEG source estimation in the HCP

- Purpose 1: spatially align MEG data to the other modalities (approximate)
- Purpose 2: achieve 'unmixing' so that connectivity estimation makes sense

# Motivation for 'unmixing'

Confounded interpretation of channel level connectivity estimates



#### Source-level connectivity: better idea



 $C(\hat{s}_1,\hat{s}_2)$ 

Note: there will still be signal leakage

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# Spatial filters are inherently blurry





# Source-level connectivity: where to look?



Source-level connectivity: start looking from locations that make sense a priori (seed-based approach)



- tMEG setting: use functionally defined seeds, e.g.
  - Sensorimotor 'voxel' showing highest coherence to reference EMG signal
  - Fusiform face area 'voxel' showing selective sensitivity to face stimuli
- rMEG setting: use fMRI RSN-based seeds

# Source-level connectivity: all-to-all approach



- Allows for investigation of full spatial structure
- Some part of the spatial structure reflect spurious connectivity

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# **Connectivity** metrics

- Many a metric on the market
- Functional versus effective connectivity
- Time domain versus frequency domain
- Frequency domain: using amplitude information versus using phase (+amplitude) information

# Spectrally-resolved C-metrics

amplitude/power (envelope) correlation

• phase difference consistency measures

• spectrally-resolved Granger causality

• cross-frequency interactions

## Why use spectrally-resolved metrics

- Oscillatory activity is a prominent feature in ongoing and event-related MEG signals
- Phase synchronisation may be an operational mechanism facilitating neuronal communication
- Overlap between topology of RSNs in fMRI with oscillatory networks observed with MEG



# Amplitude/power (envelope) correlation

- In HCP a.k.a. BLP (band-limited power) correlation
- Used as connectivity metric in the rMEG data
- Provide 'static' connectivity estimates (estimating correlation in windows, average across the whole scan duration)
- Provide 'dynamic' connectivity estimates (based on a sliding window)

#### Phase difference consistency measures way how was a second of the se MMMMM 0.0025 120 60 0.002 0.0015 HANNA WINN 150 30 0.001 180 0 210 330 240 300 37 270

### Phase difference consistency measures

- Coherence
- Phase locking value
- Imaginary part of coherency
- Phase slope index
- Phase lag index
- Weighted phase lag index



### Phase difference consistency measures

- Coherence
  - Phase locking value

Imaginary part of coherency

- Phase slope index
- Phase lag index
- Weighted phase lag index

90

270

120

240

180

210

0.0025

0.002

0.0015

0.00

60

300

30

330

0

#### Coherence

$$x_1 x_2^* = A_1 e^{i\varphi_1} \times A_2 e^{-i\varphi_2} = A_1 A_2 e^{i(\varphi_1 - \varphi_2)}$$

single trial cross-spectral density

#### Imaginary part of coherency

Coherency = 
$$\frac{1/N \sum A_1 A_2 e^{i(\varphi_1 - \varphi_2)}}{\sqrt{(1/N \sum A_1^2)(1/N \sum A_2^2)}} = e^{i(\varphi_1 - \varphi_2)}$$



#### Imaginary part of coherency



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# Parcellations and MEG

- Motivation: dimensionality reduction
  - Number of independent sources estimable per timeslice is limited anyway: <250</li>
  - 'smoothing' of spatial noise
  - Allows for manageable-sized time-resolved connectivity matrices
- Challenge: optimal parcellation is unknown
  - Likely depends on data
  - When (in the course of analysis pipeline) to parcellate?
- Next MEG release: parcellation of connectomes based on the Yeo 2011 paper (functional parcellation based on resting state connectivity)



#### Thanks for listening