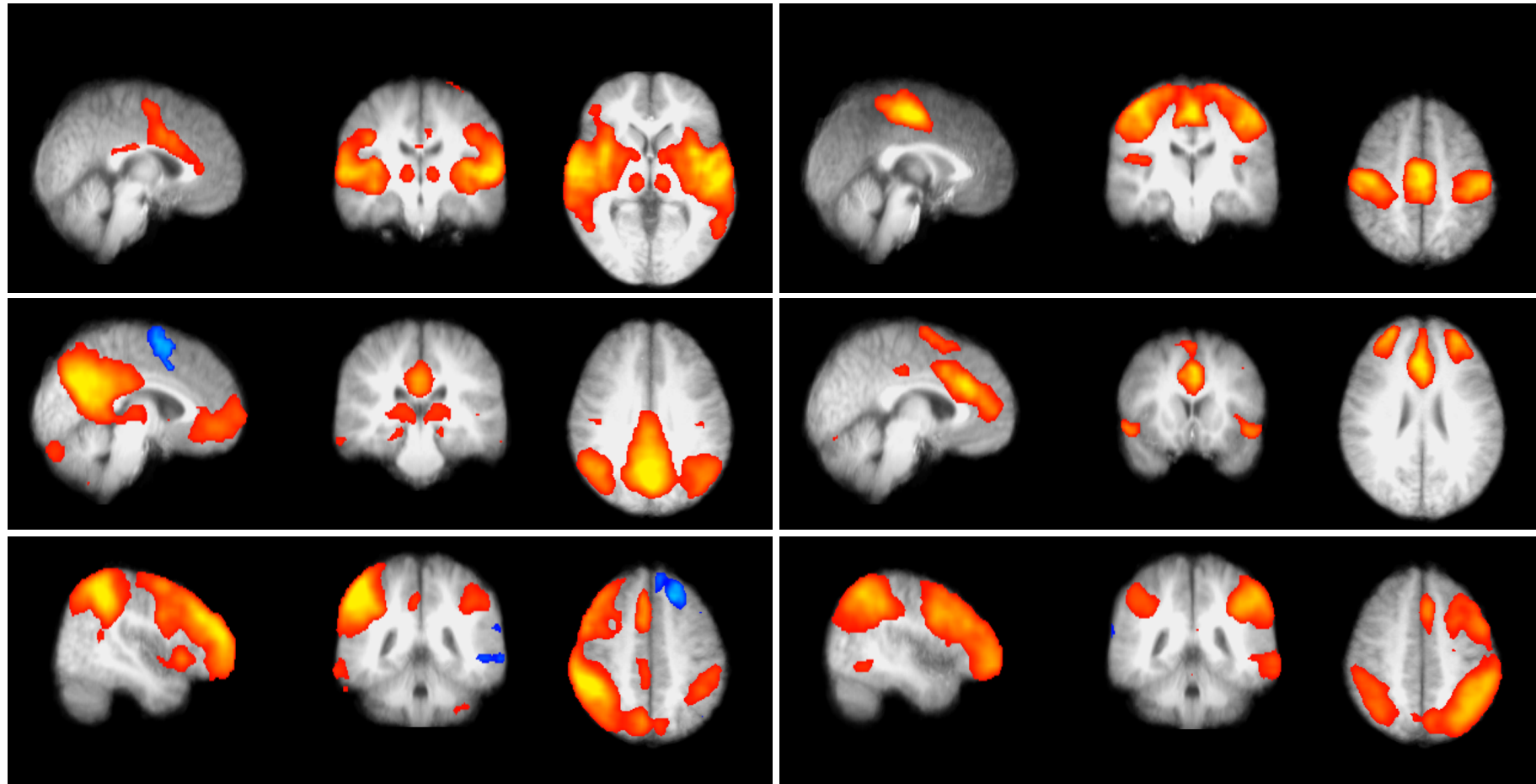


HCP Course 2015

rfMRI background, preprocessing, denoising

Stephen Smith, FMRIB Oxford

Resting-State Networks

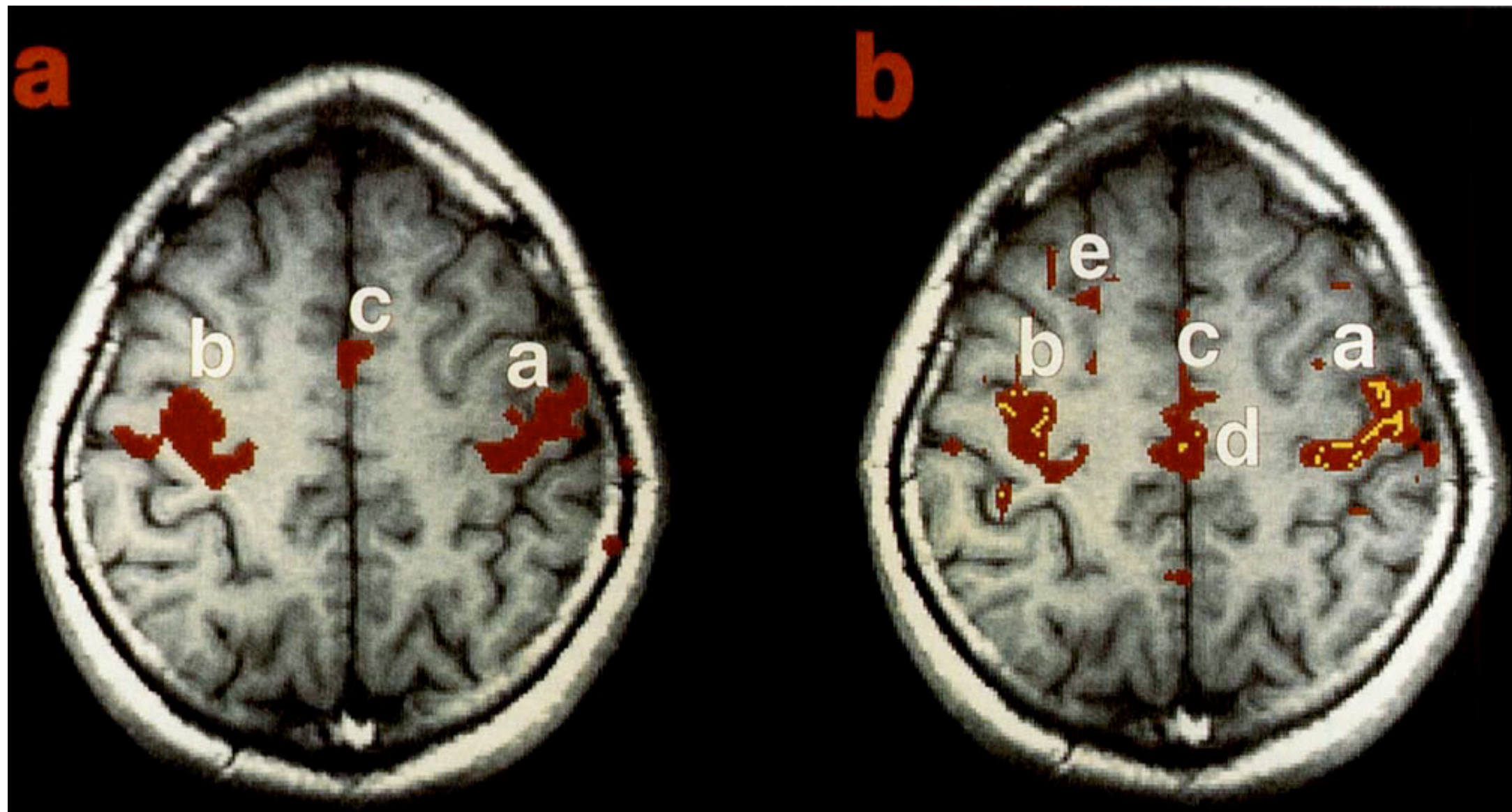


- *Spatial patterns* of correlated temporal dynamics, resembling activation maps
- can be found in fMRI data (BOLD & ASL) obtained under stimulation *and* in resting data
- often described as having low frequency power spectra

Correlations in spontaneous temporal fluctuations

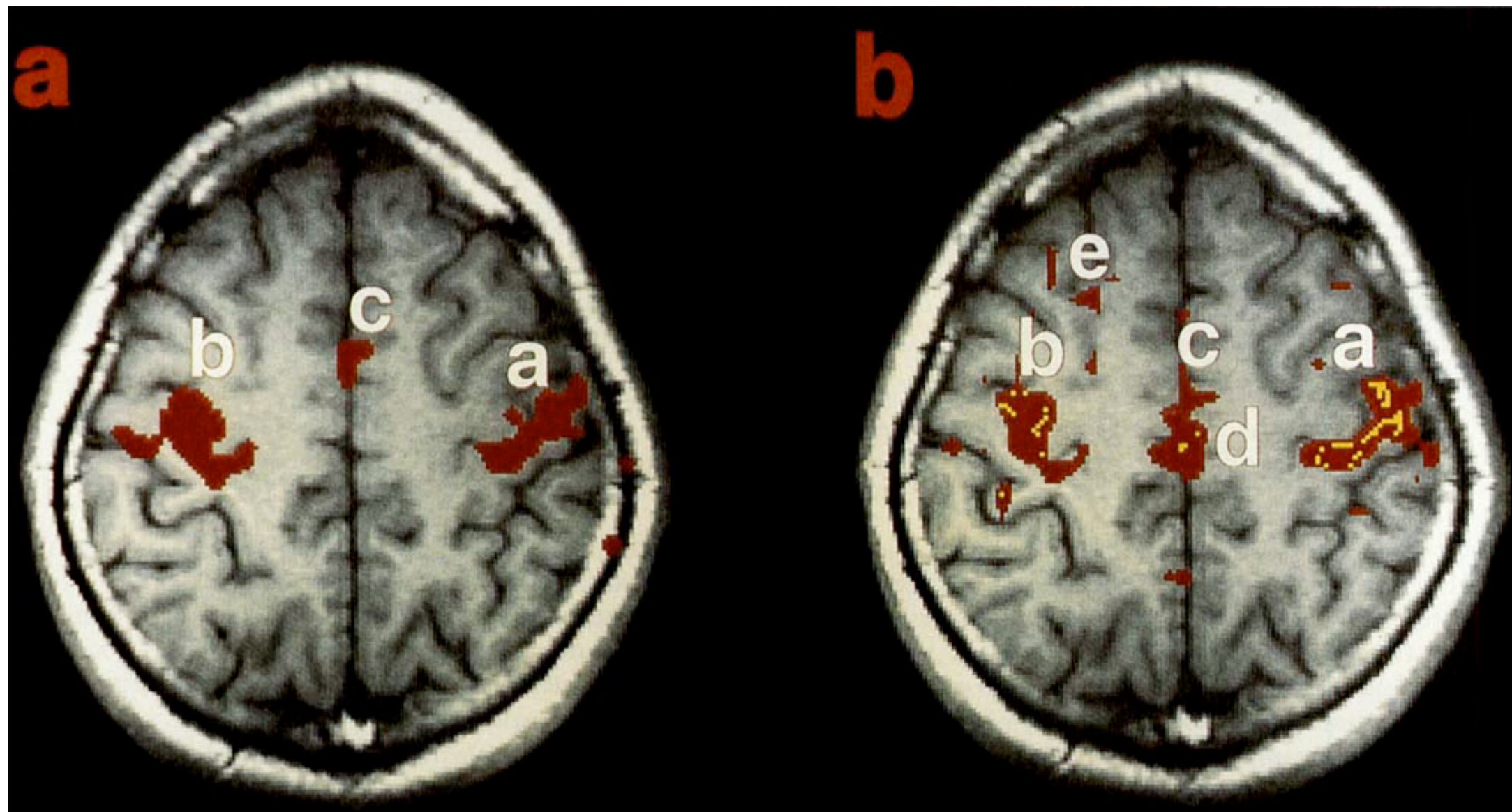
Activation maps from a
finger tapping experiment

Correlation maps from a
resting state experiment



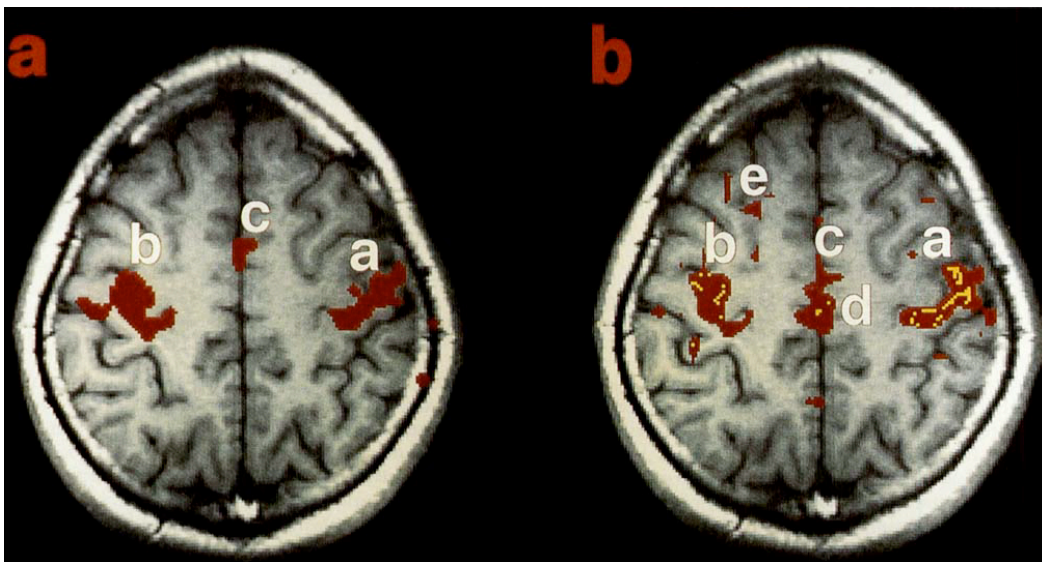
Spontaneous correlations = functional connectivity?

- Two areas correlate because they are functionally linked
- Not surprising that this is seen in “resting” data



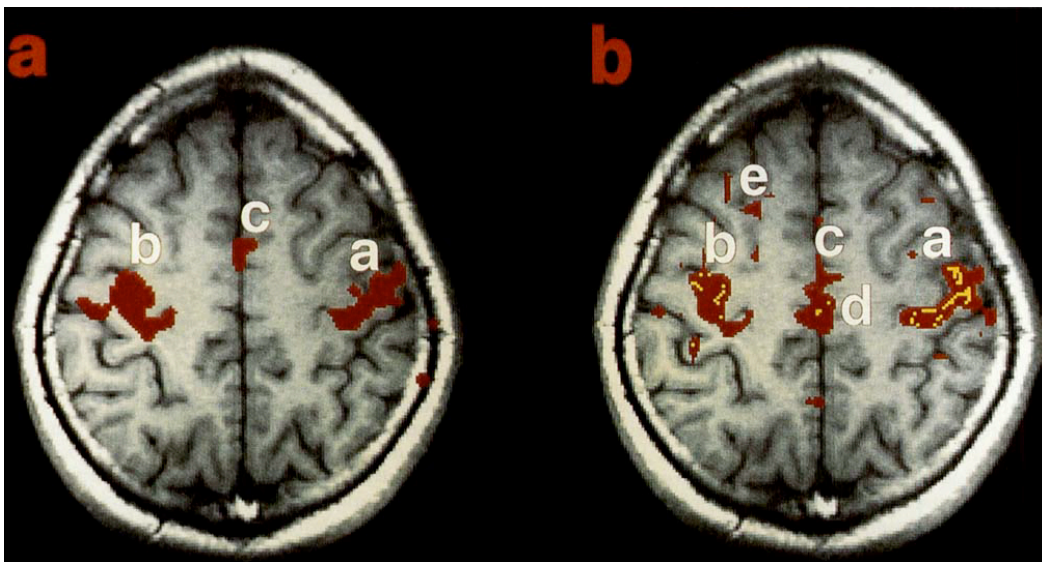
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- “functional connectivity” = correlation
= direct or indirect connection
- “effective connectivity” = direct/causal connection



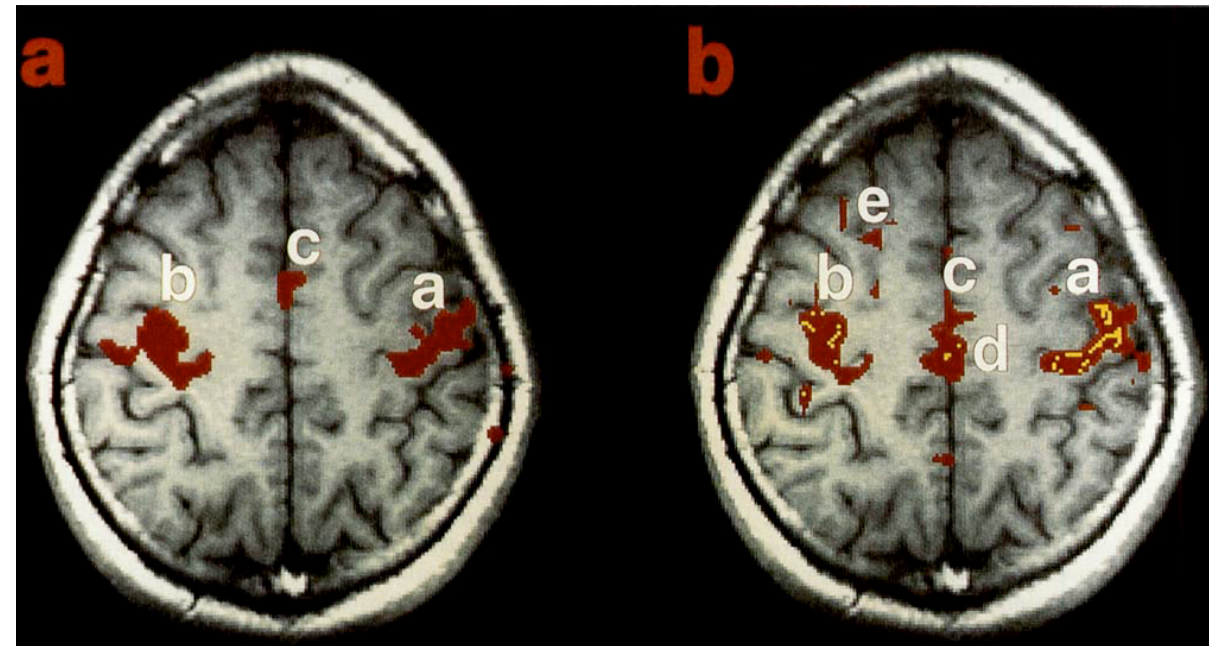
Spontaneous correlations = functional connectivity?

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- “functional connectivity” = correlation
= direct or indirect connection
 - easy to estimate, less meaningful
- “effective connectivity” = direct/causal connection
 - more meaningful, harder to estimate

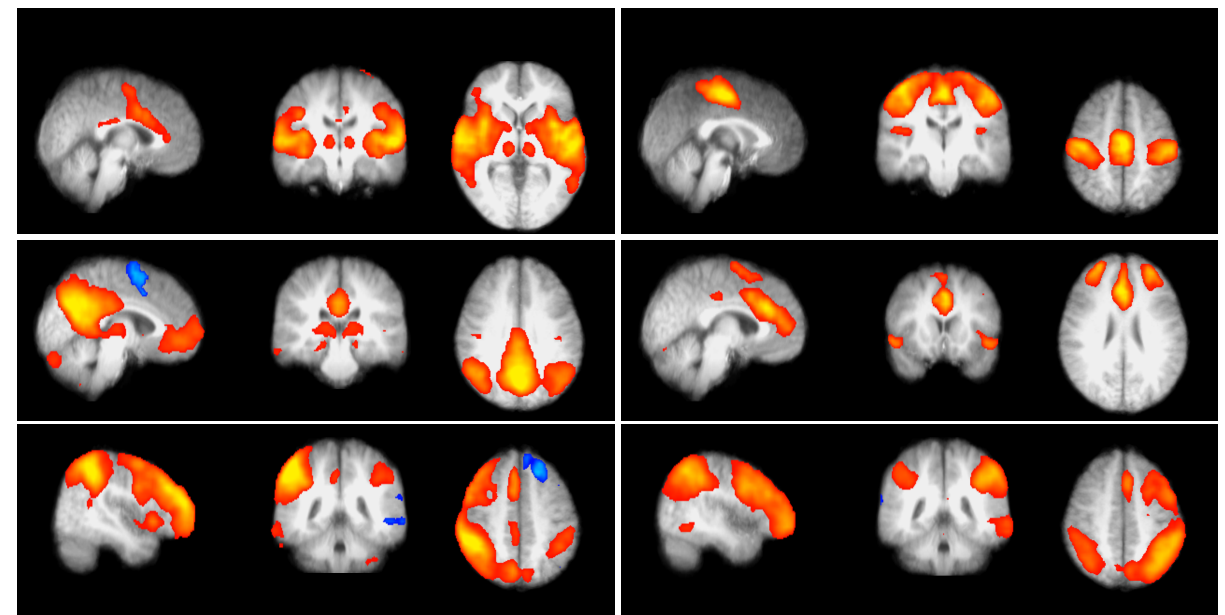


Popular methods for analysing resting FMRI data

- Seed-based correlation

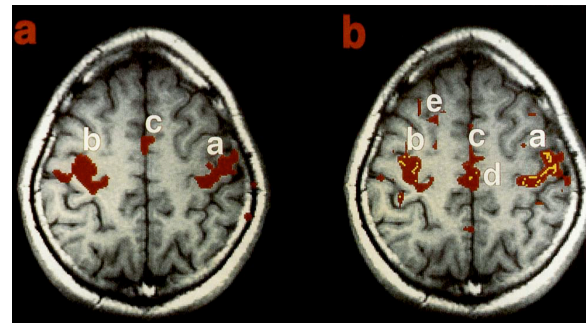


- ICA(independent component analysis)

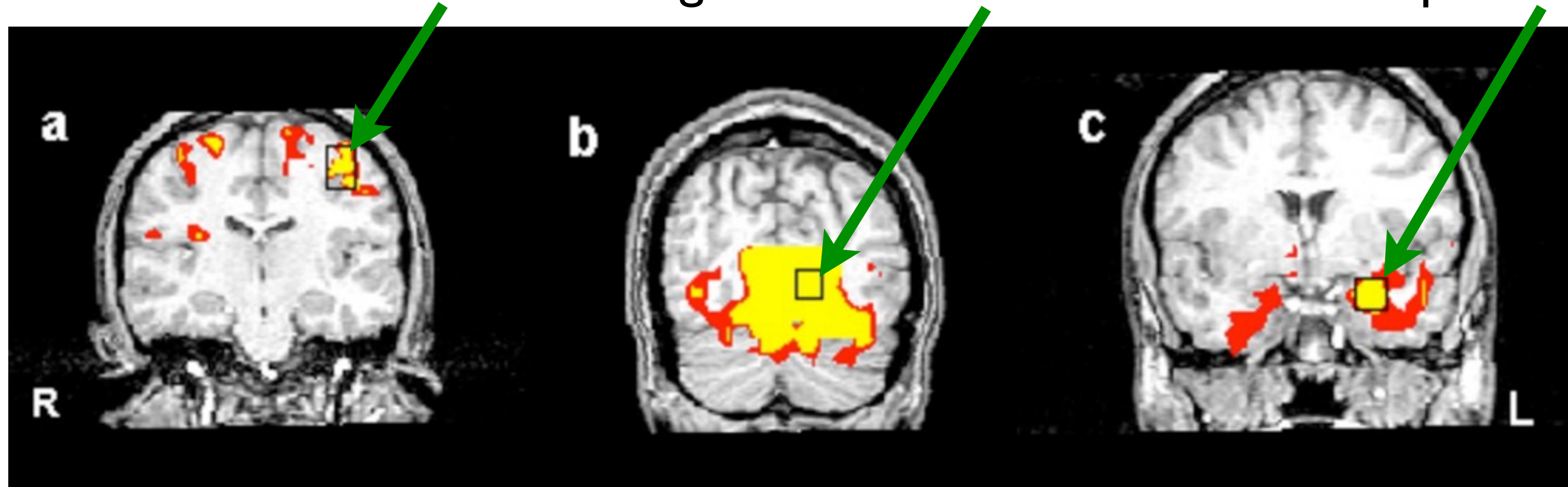


- review papers
 - Calhoun *NeuroImage* 2008
 - Cole *Frontiers Sys Neur* 2010

- Seed-based correlation

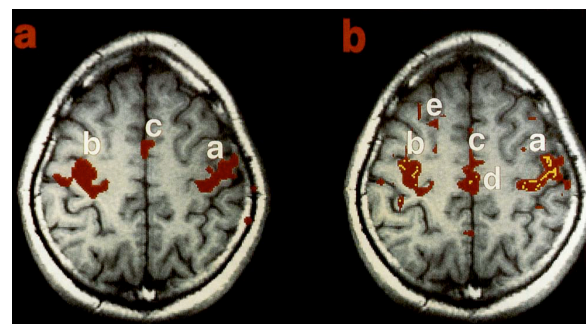


- Different seed locations generate different correlation maps

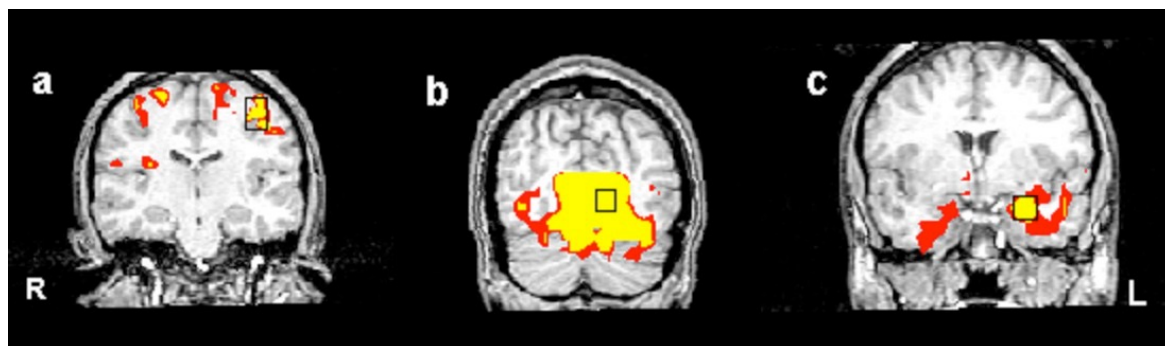


- *Lowe NeuroImage 1998*

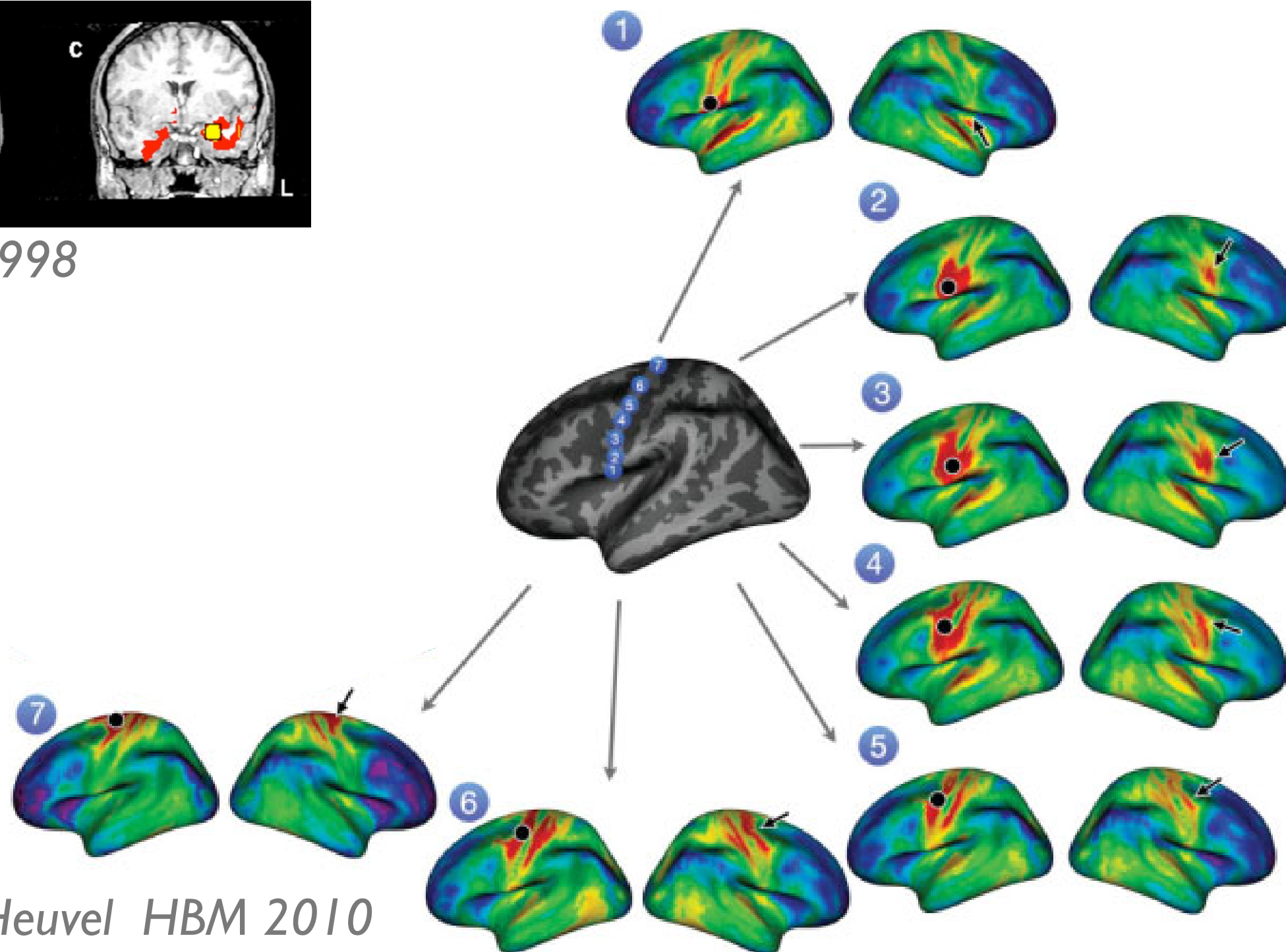
- Seed-based correlation



- Different seed locations generate different correlation maps



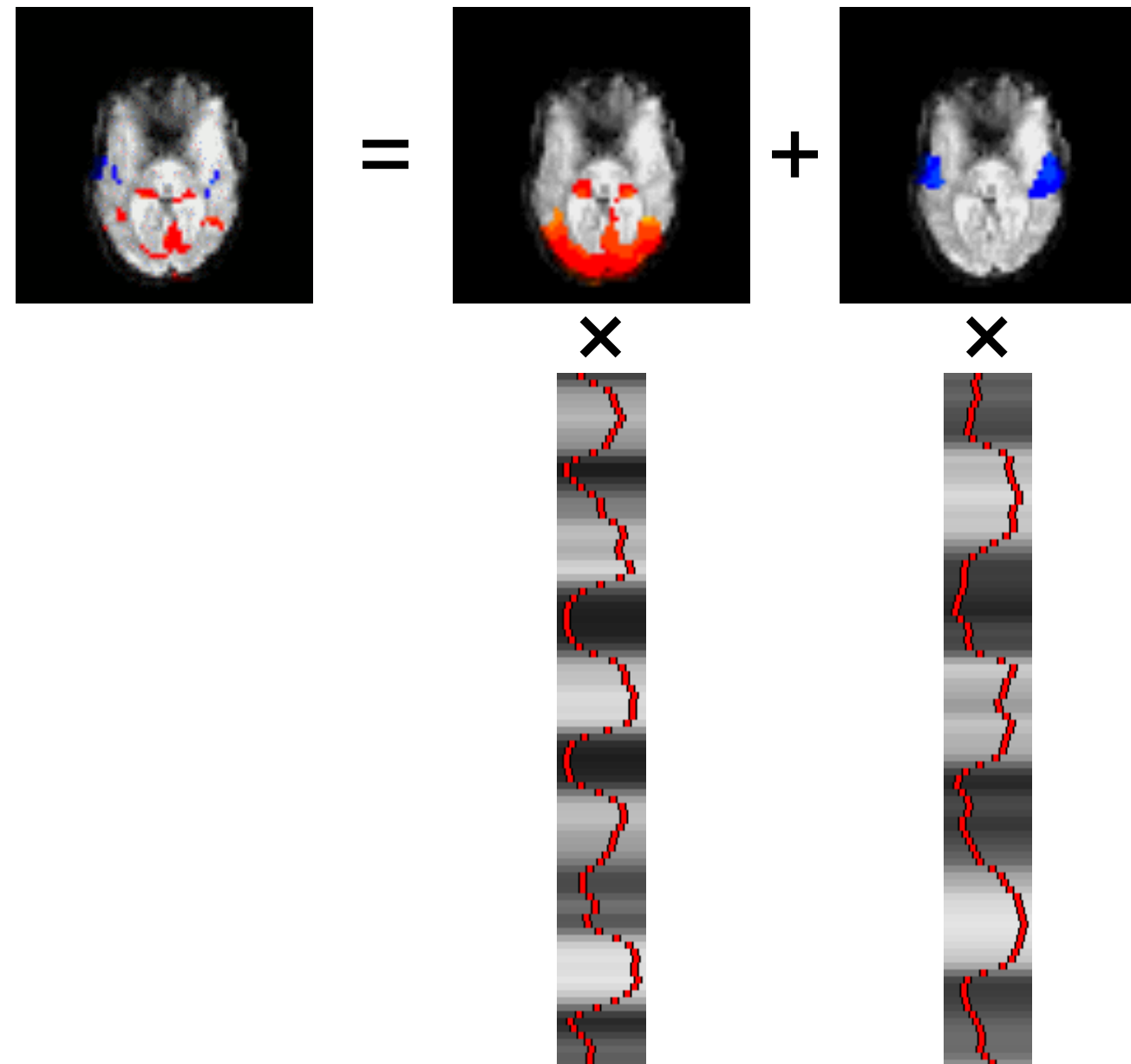
- *Lowe Neurolmage 1998*



- *van den Heuvel HBM 2010*

ICA

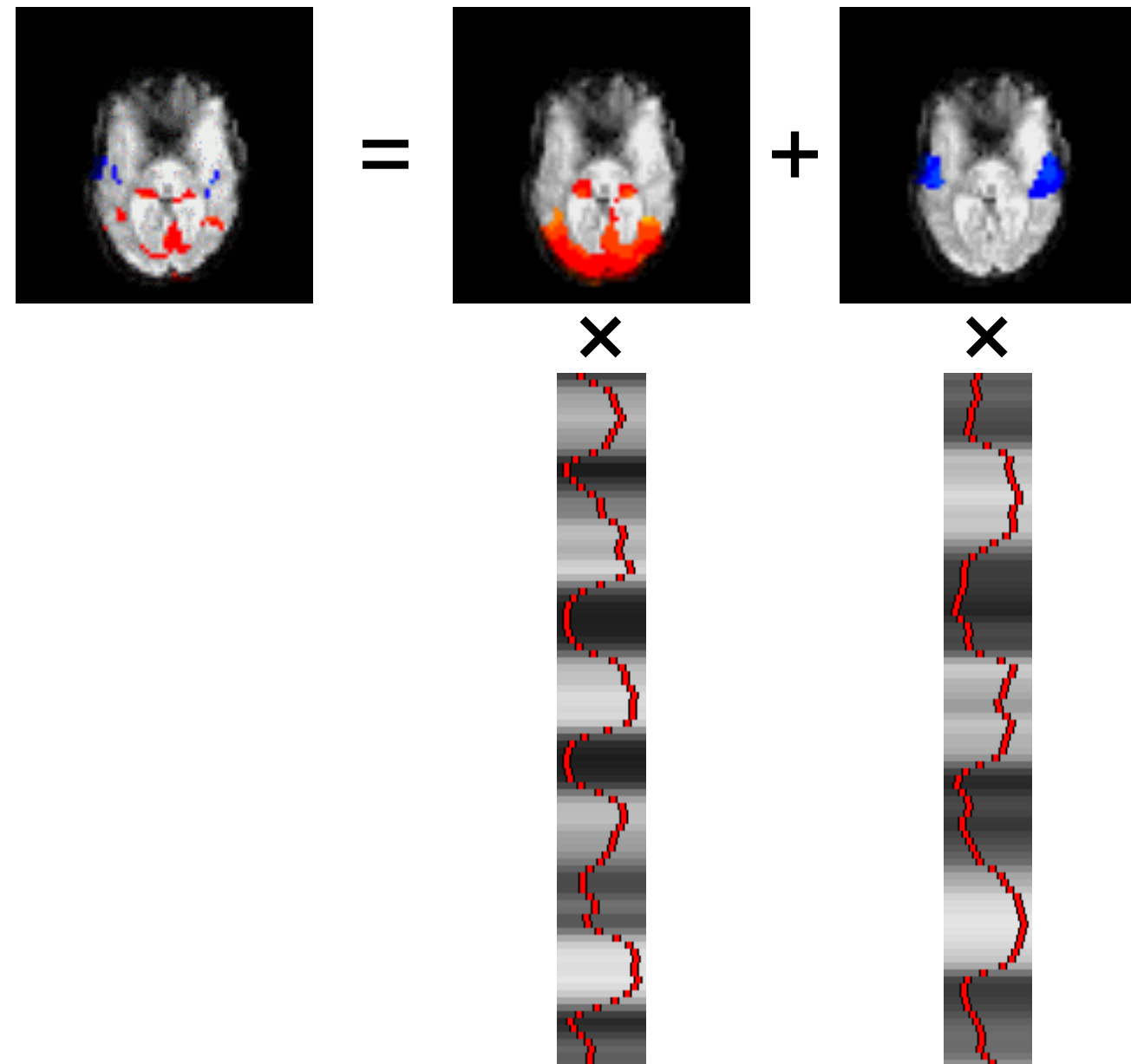
ICA decomposes data into a set of distinct spatial maps, each with its own distinct timecourse



- *ICA*
 - *Comon Signal Processing 1994*
 - *Bell Neural Computation 1995*
- *ICA for fMRI*
 - *McKeown Human Brain Mapping 1998*
- *ICA for resting fMRI networks*
 - *Kiviniemi Neurolmage 2003*
- *ICA for fMRI - software*
 - *MELODIC in FSL (Beckmann)*
 - *GIFT (Calhoun)*
 - *BrainVoyager (Formisano)*

ICA

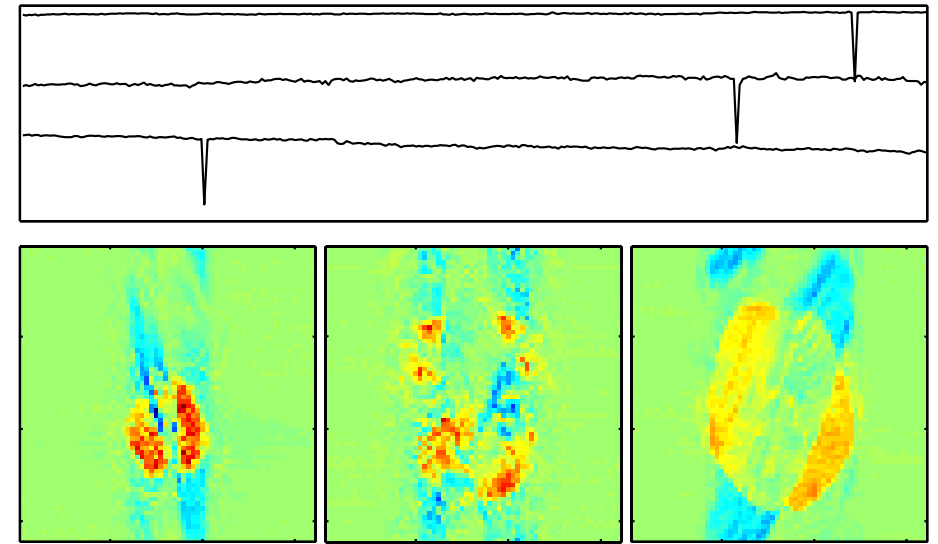
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Good for finding:

- Scanner and physiological artefacts
- Activation
- Resting networks

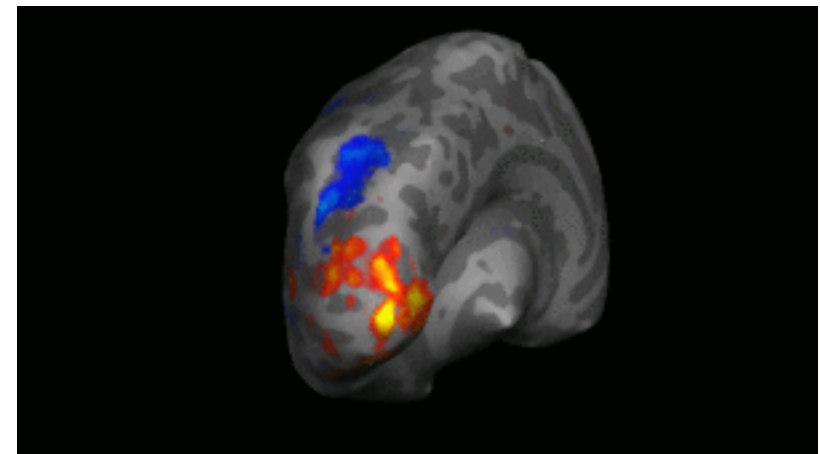
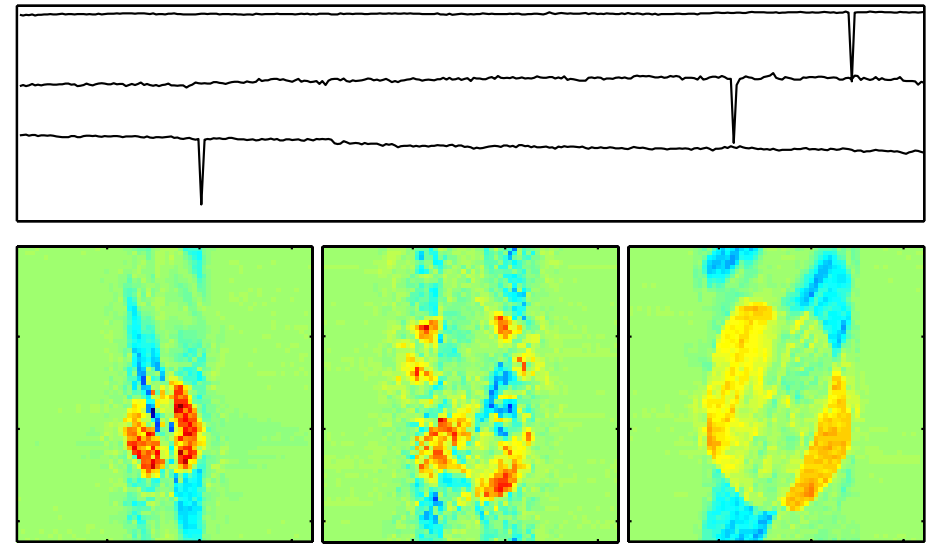
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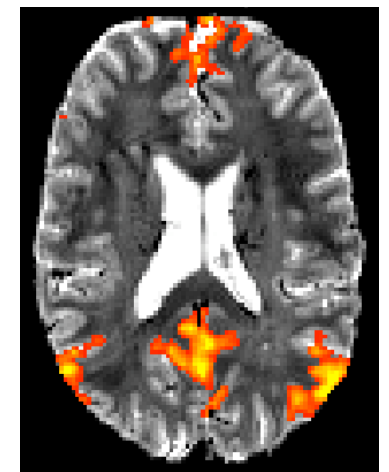
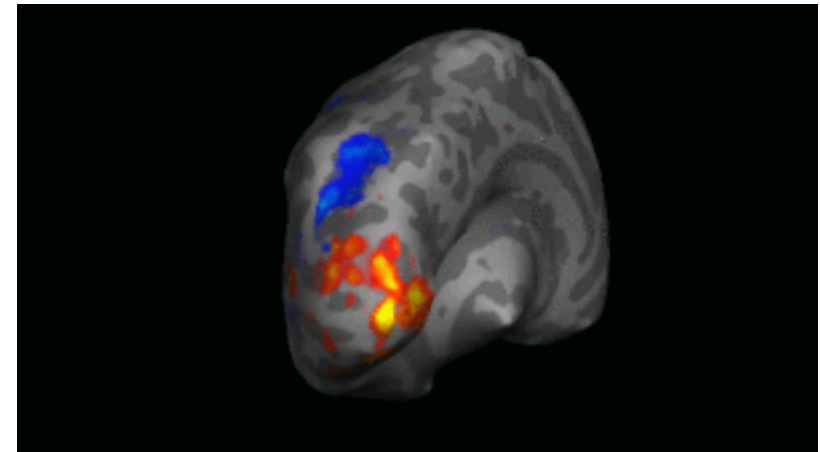
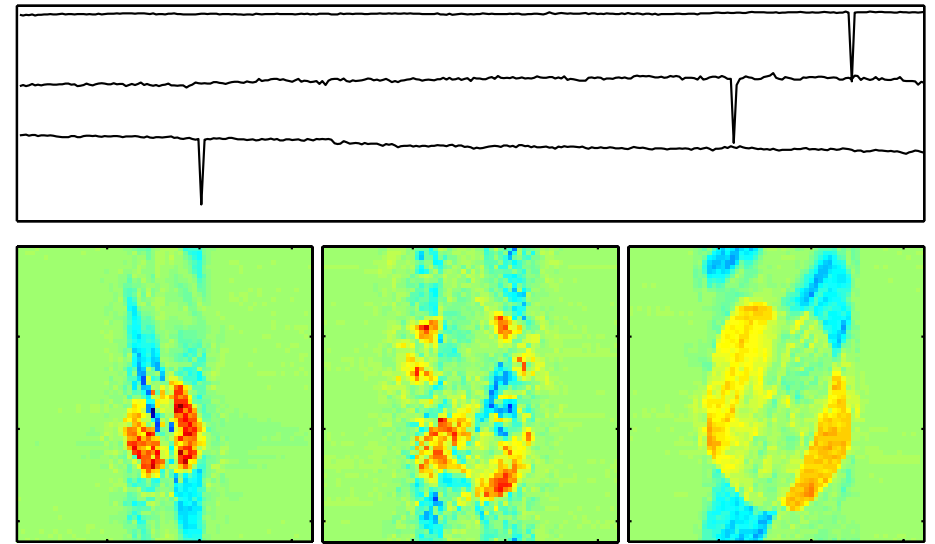
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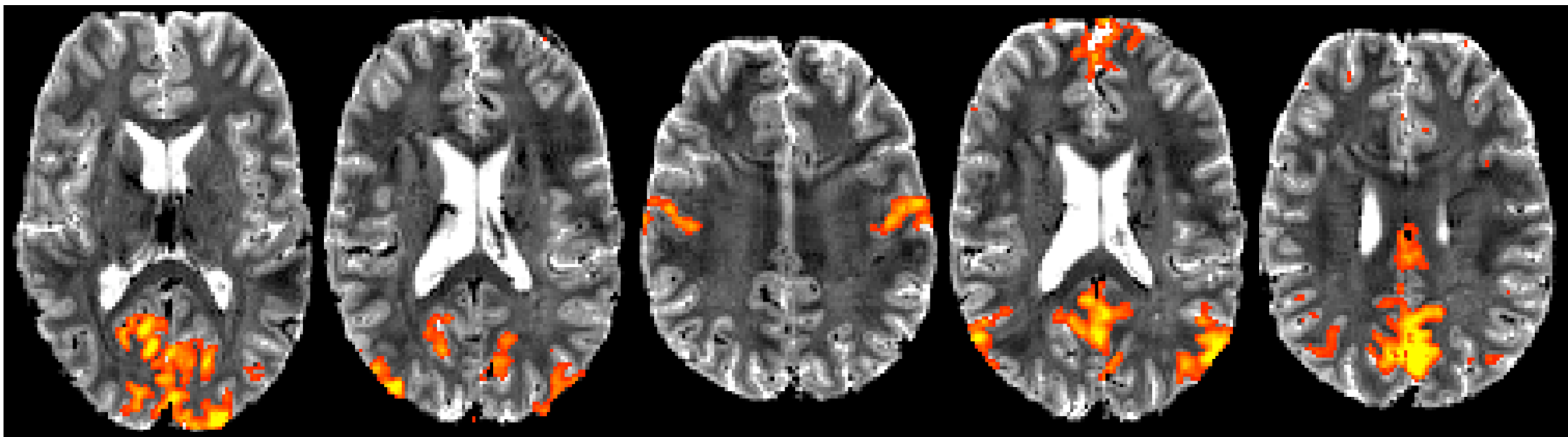
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Seed-based correlation vs. ICA

- Seed-based
 - Good: allows you to ask a straightforward question and get an easily interpretable answer
 - Bad: only tells you about the seeds you ask about (though see Cohen's gradient-based parcellation)
- ICA
 - Bad: some components can be hard to interpret, and you may not get a component that clearly relates to the brain-bit you cared about
 - Bad: run-run variability in decomposition (but see ICASSO)
 - Good: the entire dataset is decomposed into “all” the different networks present

Spatial characteristics

- RSNs - multiple grey-matter networks

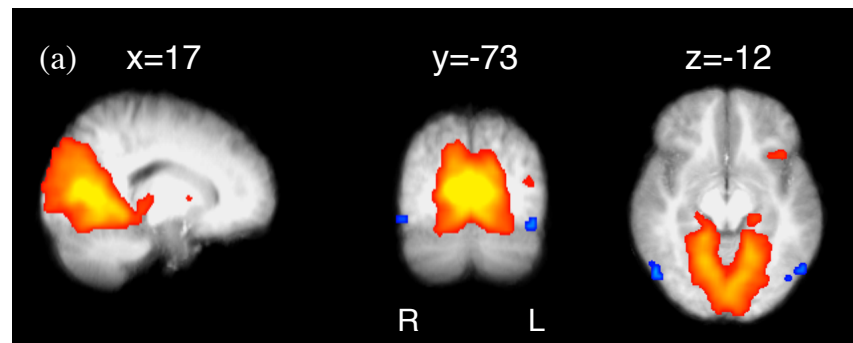


- Human Connectome Project pilot data (7T, 1.5mm, 6mins)
(U Minnesota, E Yacoub & K Ugurbil)

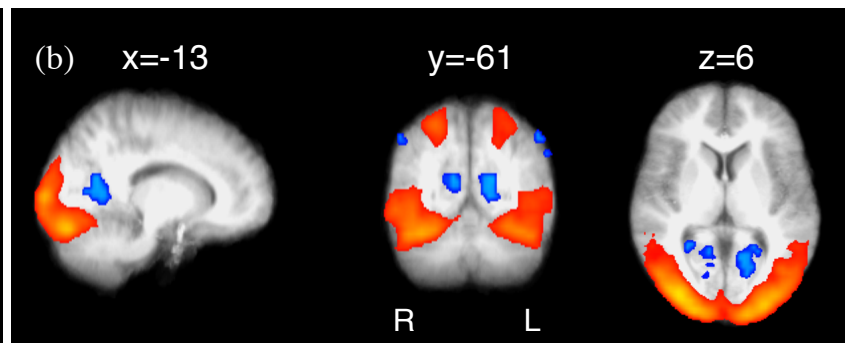
Spatial characteristics

Low-dimensional (~ 20) ICA gives distinct “resting state networks”

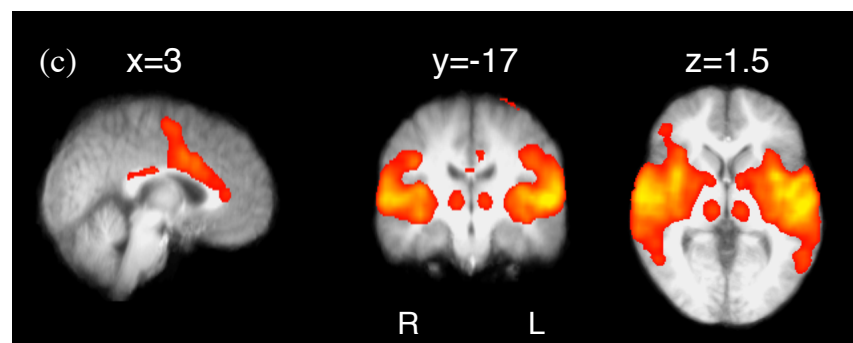
medial
visual



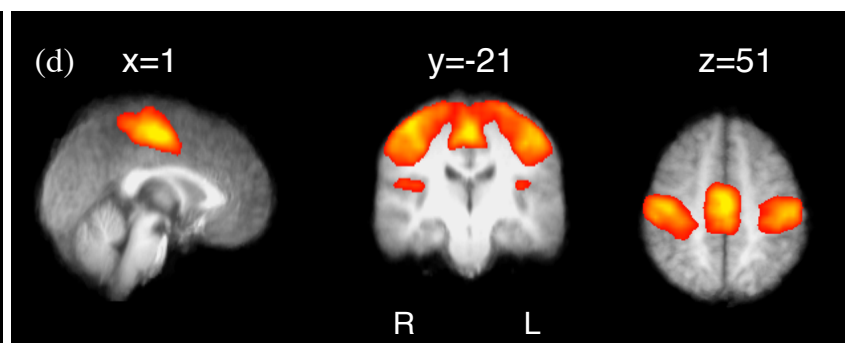
lateral
visual



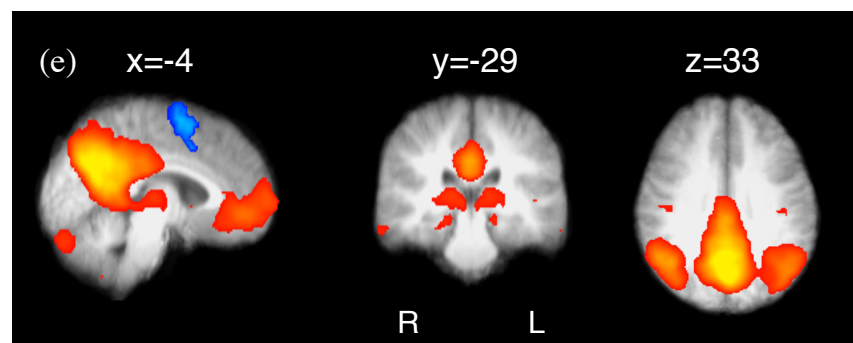
auditory



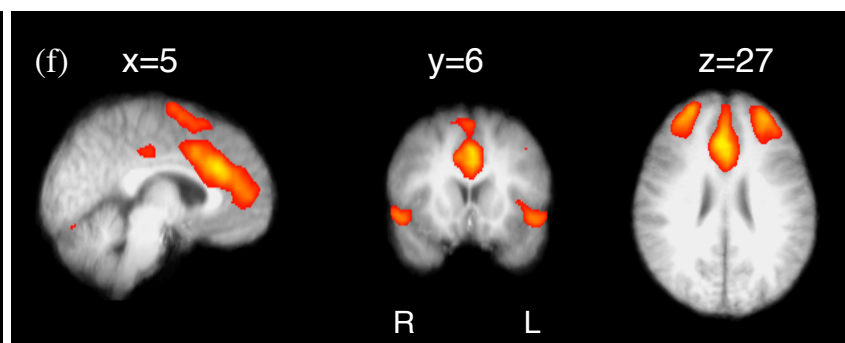
sensori-
motor



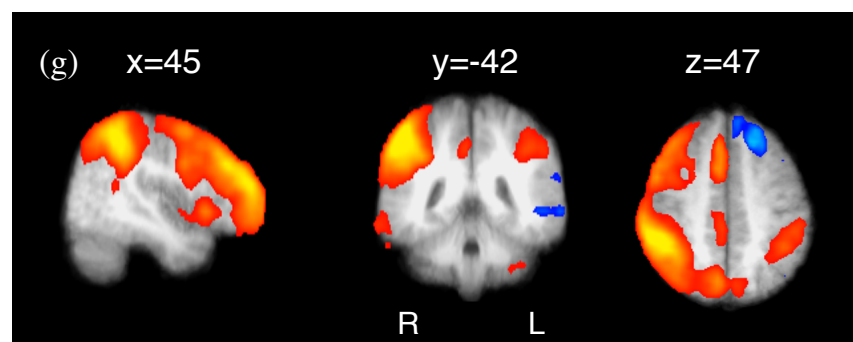
default
mode



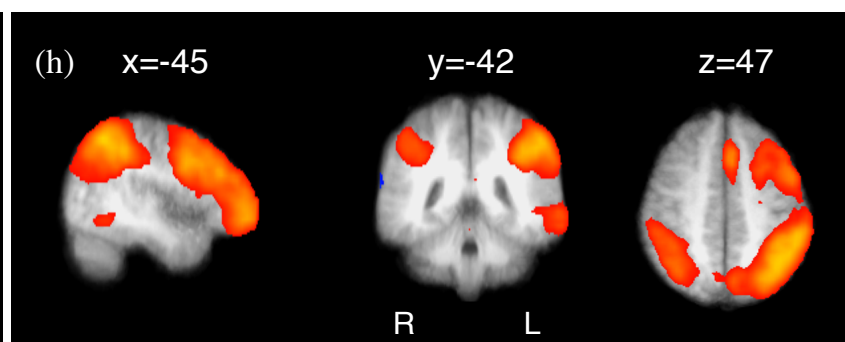
executive



right fronto-
parietal



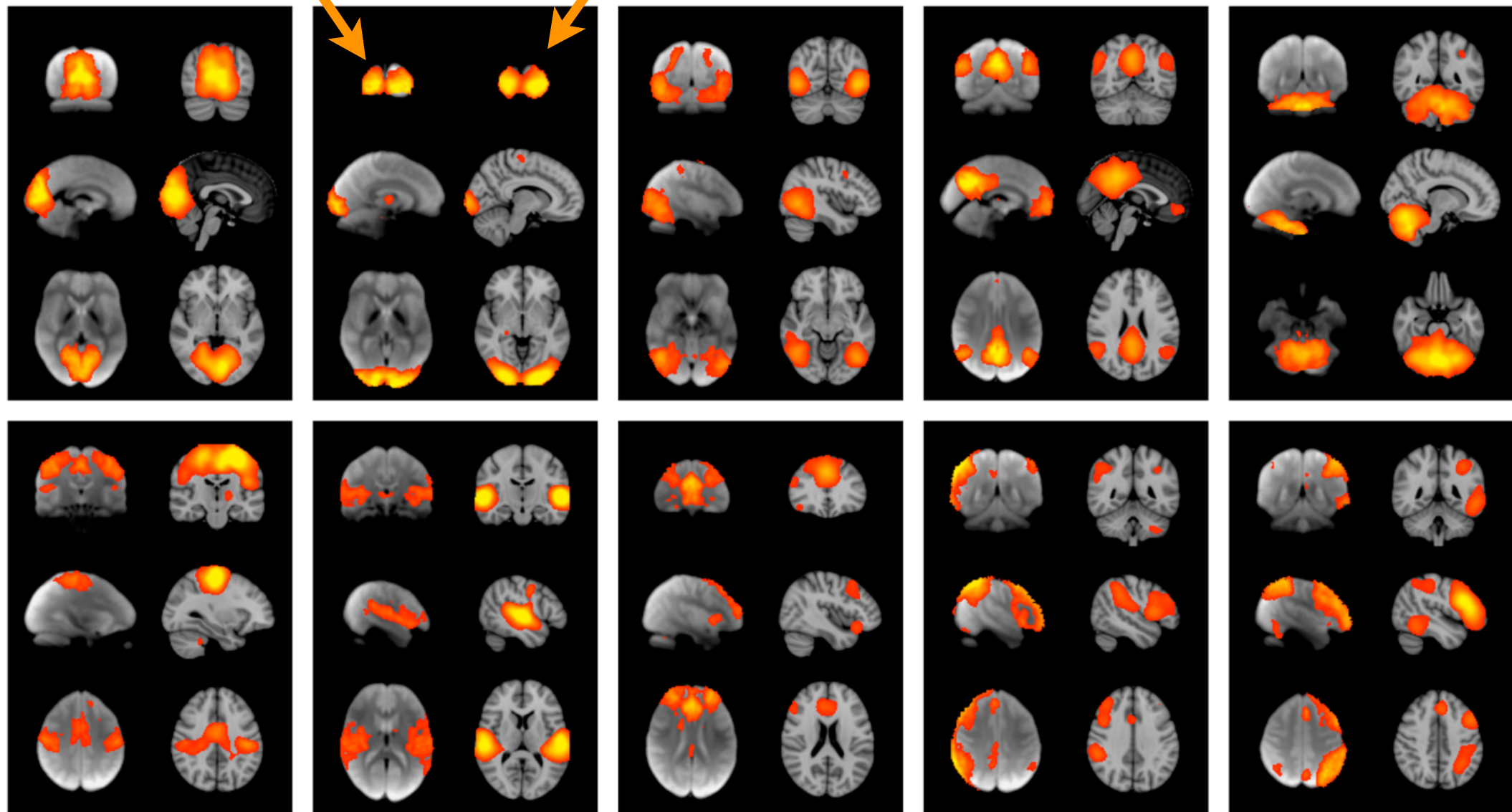
left fronto-
parietal



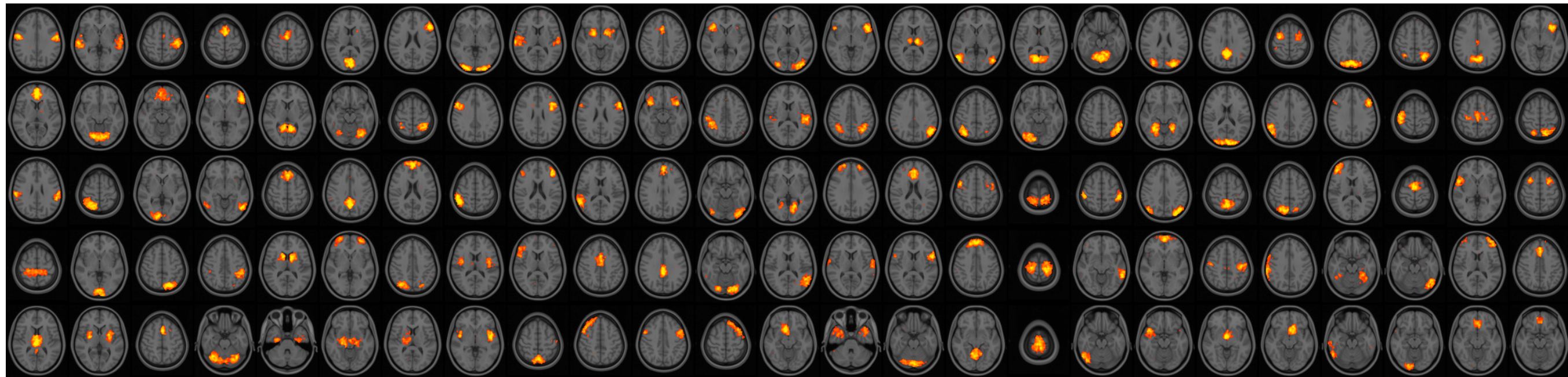
Correspondence between resting FMRI and task-activation studies

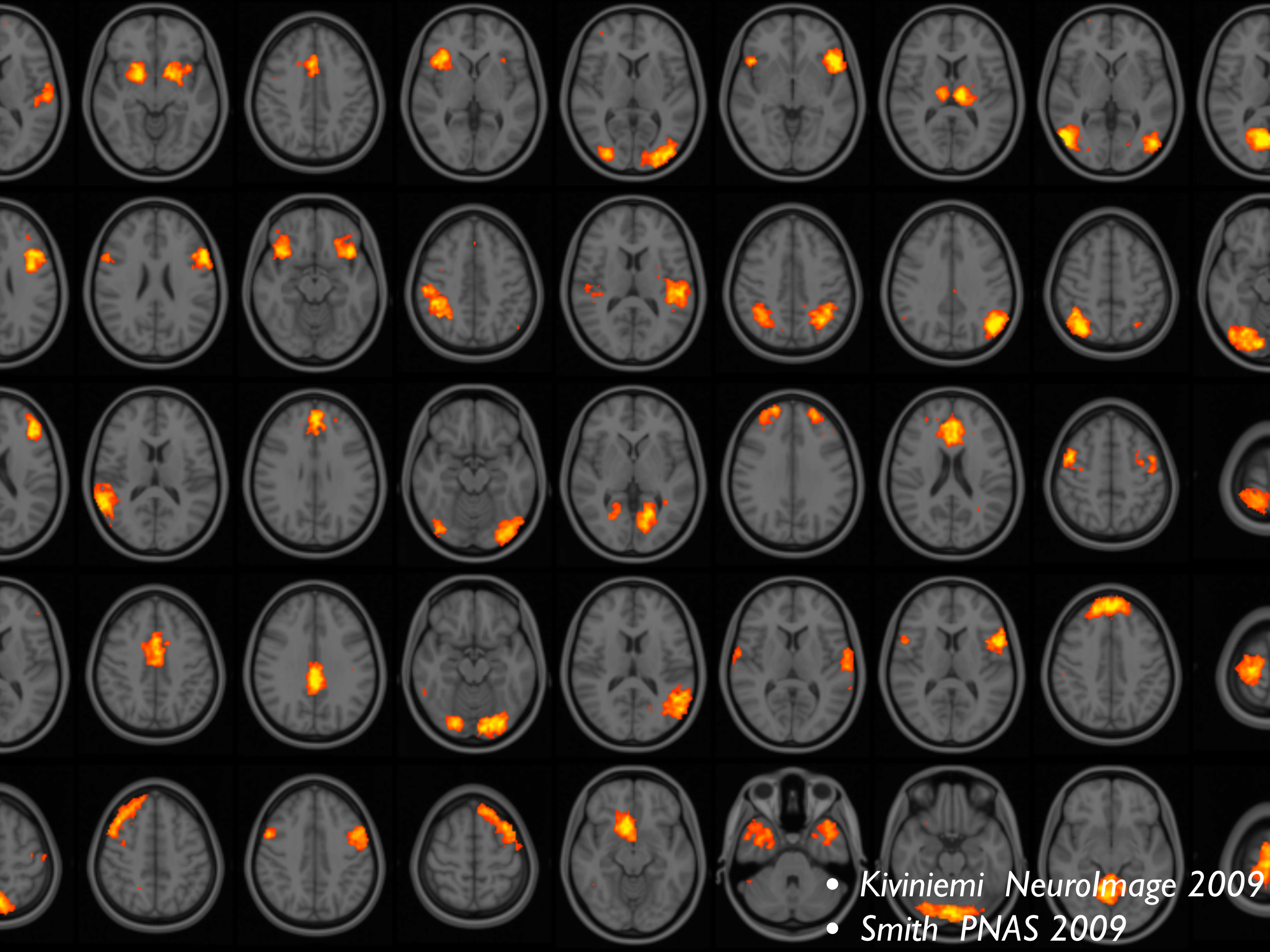
one component
from group-ICA
on 36-subject
resting FMRI

one component from ICA
on activation images from 1687
task studies in the San Antonio
BrainMap meta-database



High-dimensional (~ 200) ICA gives a “parcellation”

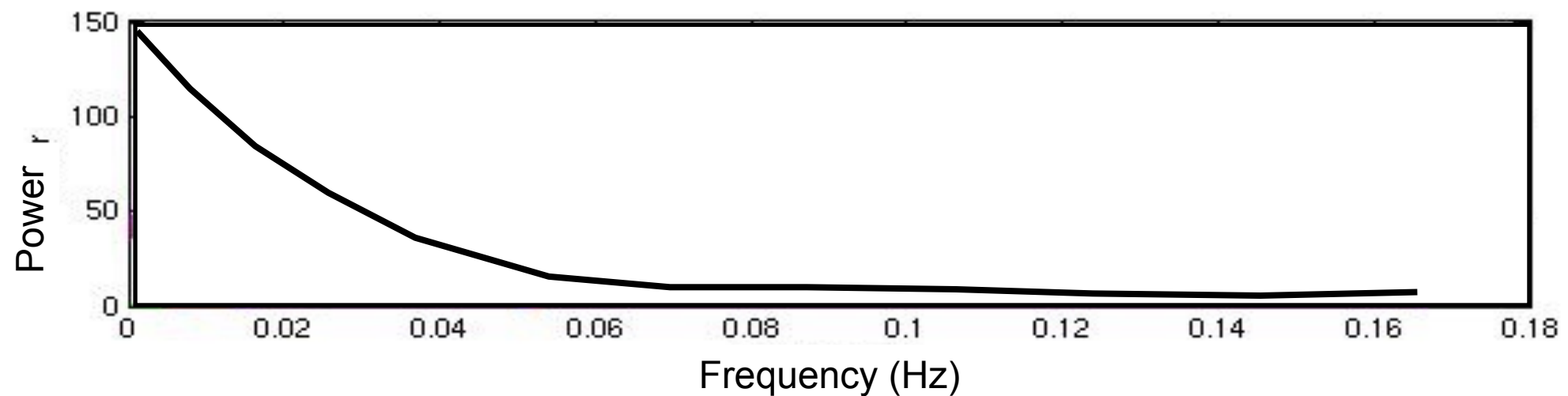
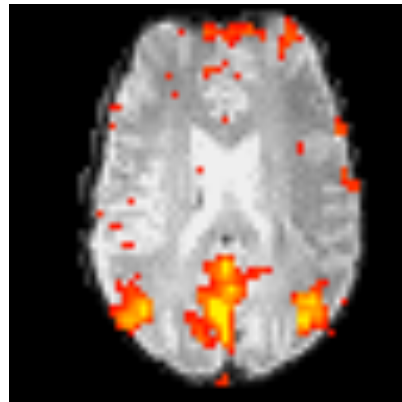




- Kiviniemi Neurolmage 2009
- Smith PNAS 2009

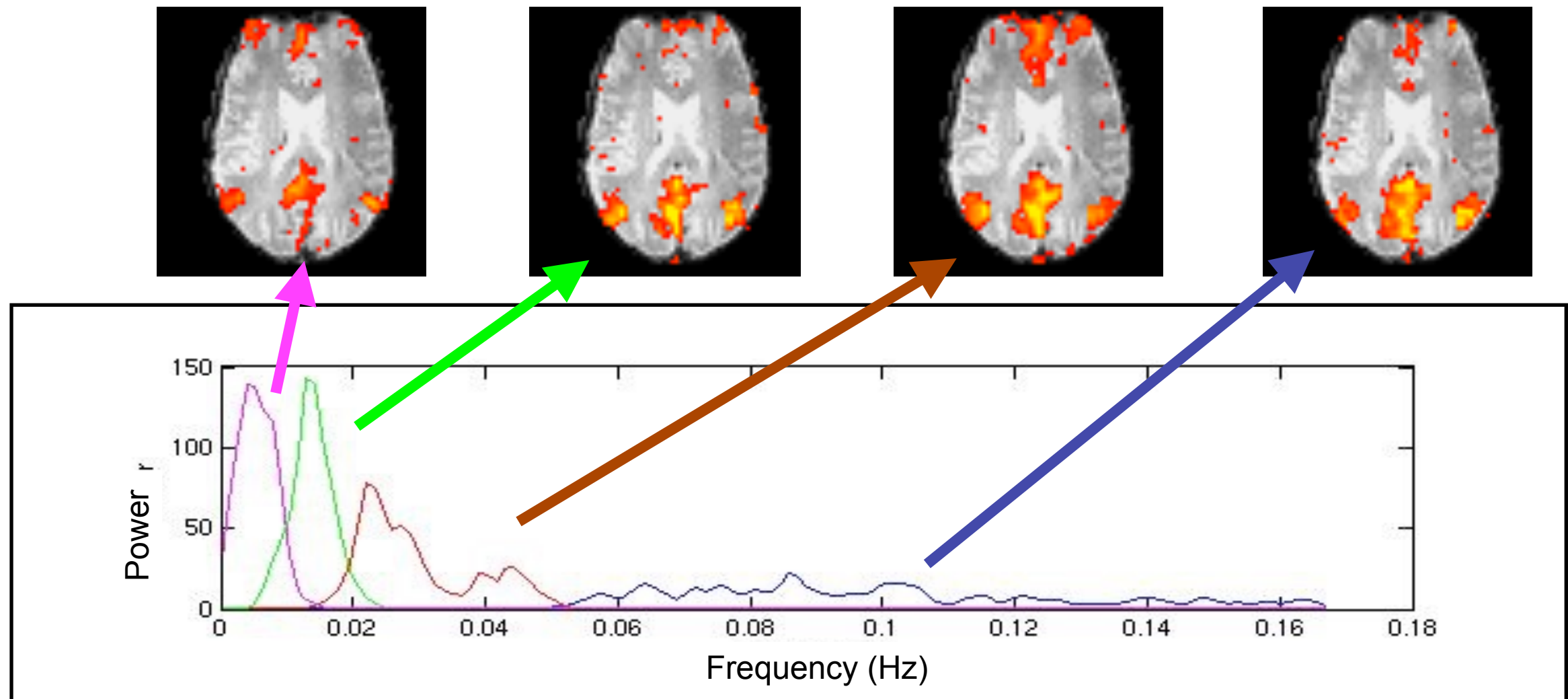
Temporal characteristics

- Generally described as “low frequency” or “1/f”

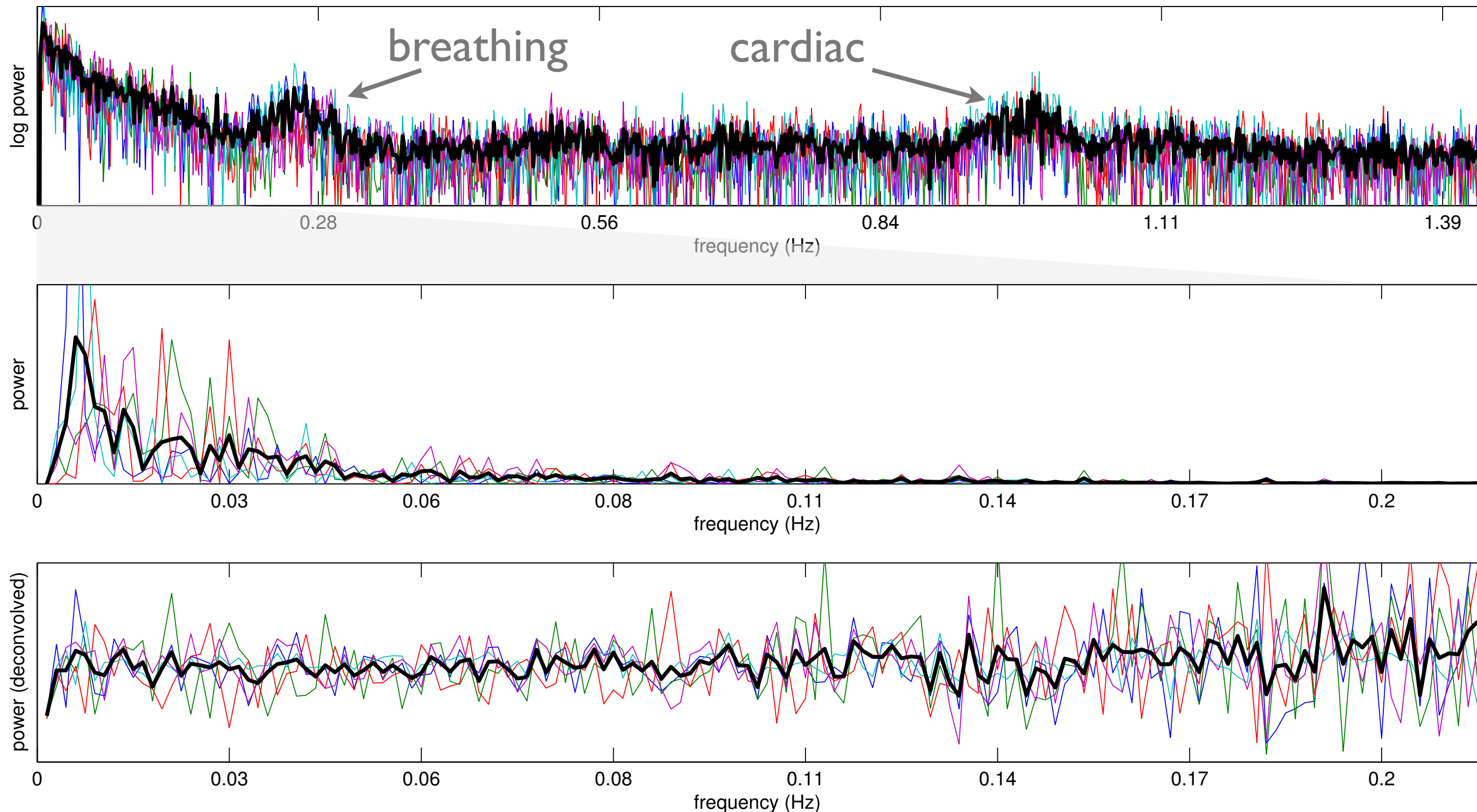


Temporal characteristics

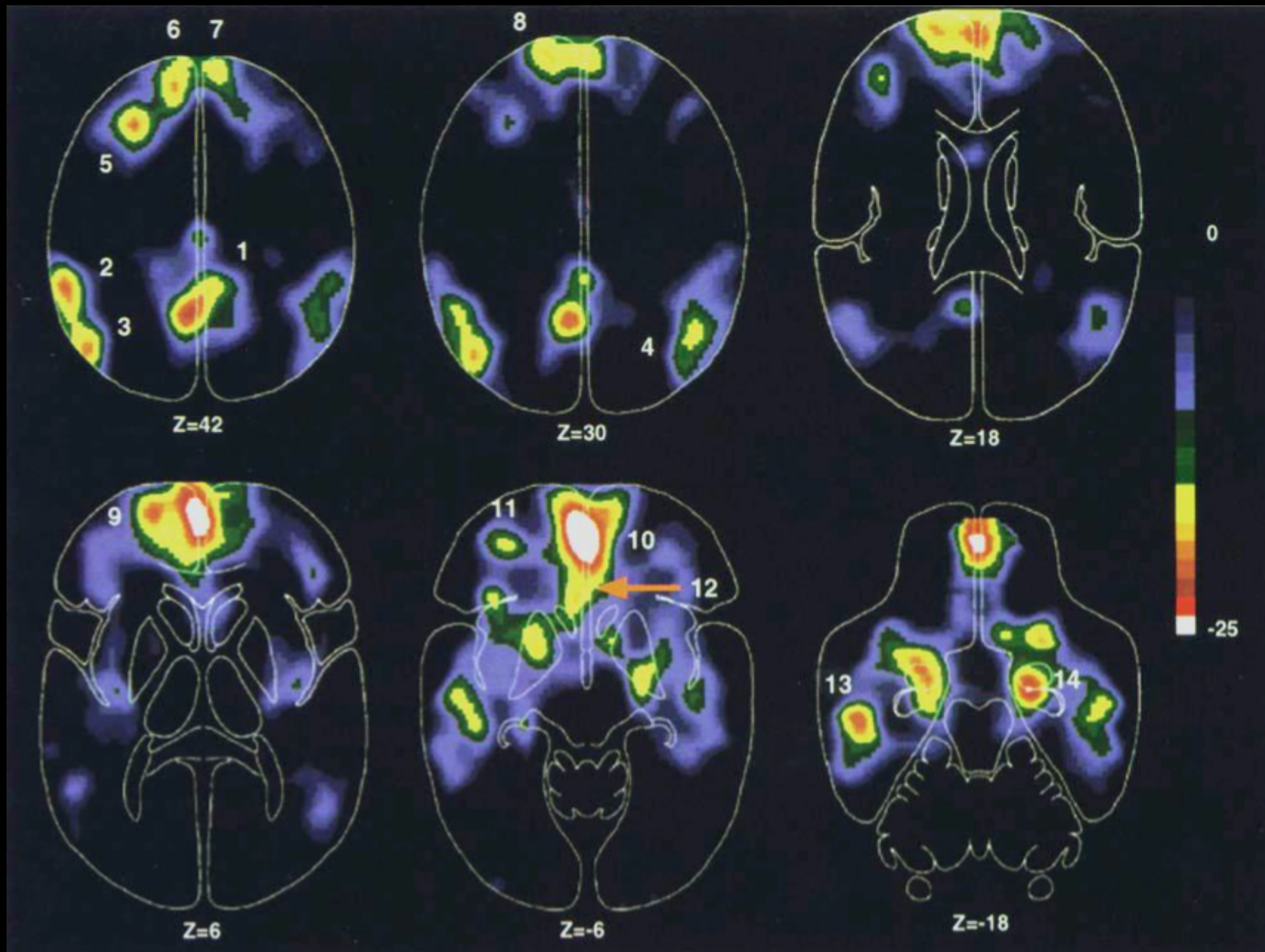
- Generally described as “low frequency” or “1/f”
- Split frequency spectrum into four bands and run ICA on each
- Suggests RSNs are broadband processes temporally



- Top: Power spectra from 5 RSNS (TR=0.35s).
- Middle: Spectra suggest RSNs in BOLD are “low frequency” (or “1/f”)
- Bottom: Deconvolve HRF in original data - now flat up to 0.2Hz



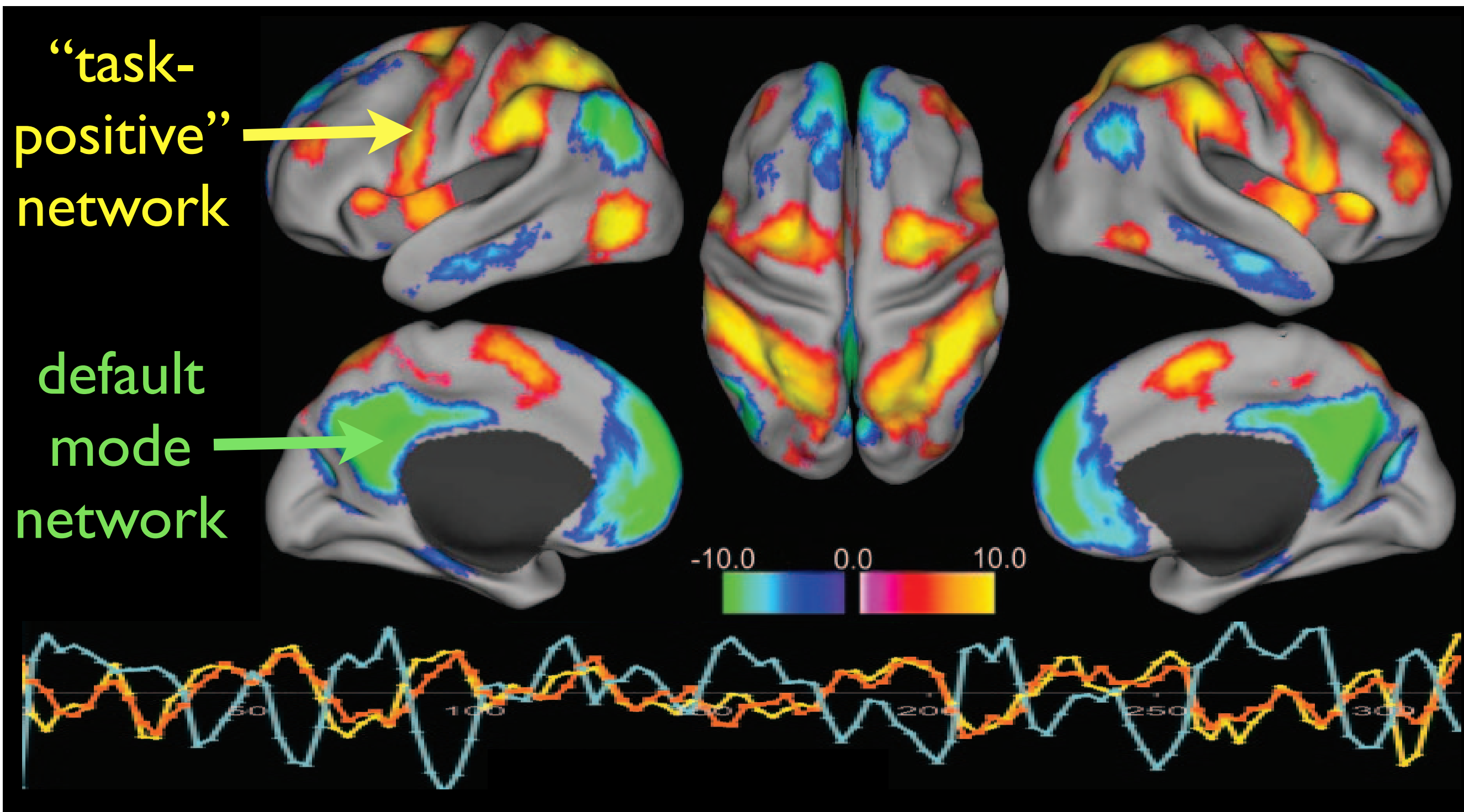
Anti-correlated networks



“Default mode network” - a network that deactivates during many activation studies

- Shulman JCN 1997
- Raichle PNAS 2001

Anti-correlated networks



“Default mode network” and “task-positive network” are anticorrelated in resting data

- Fox *PNAS* 2005
- Fox *J Neurophys* 2009

rfMRI artefacts & cleanup

- Structured artefacts *much* more of a problem for rfMRI than task-fMRI (*because it's based on correlating timeseries with each other rather than an "external" timeseries - that in general will not be correlated with these confounds*)
 - Head motion
 - Cardiac & breathing cycles
 - Scanner artefacts

rfMRI artefacts & cleanup

- Estimate “confound” timeseries; regress these out of the data:
 - External physiology measurements (RETROICOR)
 - rfMRI-data-derived measurements
 - head motion parameters
 - white-matter / CSF / whole-brain mean timeseries
 - ICA artefact component timeseries
- Highpass / lowpass temporal filters
- “Scrubbing” (delete bad timepoints)

temporal filtering

- Highpass temporal filtering
 - E.g., remove frequencies < 0.001 Hz
 - Reasonable to remove slowest data drifts
- Lowpass temporal filtering
 - E.g., common to remove frequencies > 0.1 Hz
 - May remove useful signal
 - Not guaranteed to remove much artefact
 - Maybe a “last resort” if other options not available

To demean or Not to demean?

- What about “global signal removal” (mean timecourse over whole brain)?
 - Another source of noise that’s good to remove ... ?
 - But what if it contains some “neural” signals of interest?
 - Makes it hard to interpret whether different networks are positively / negatively correlated
 - Fox (J Neurophysiol, 2009), Murphy (NeuroImage 2009), etc.

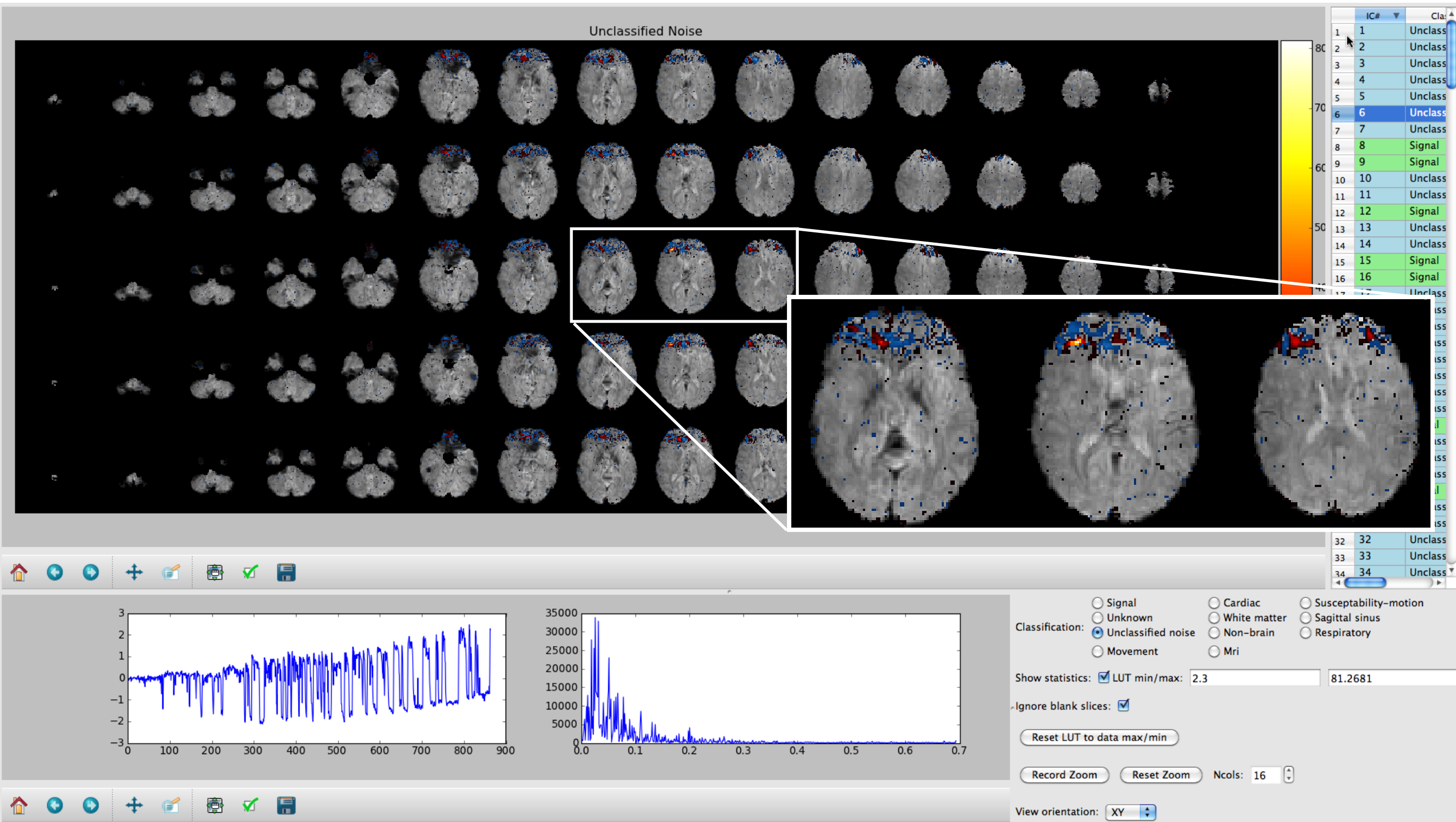
FIX (FMRIB's ICA-based X-noiseifier)

Salimi-Khorshidi NeuroImage 2014

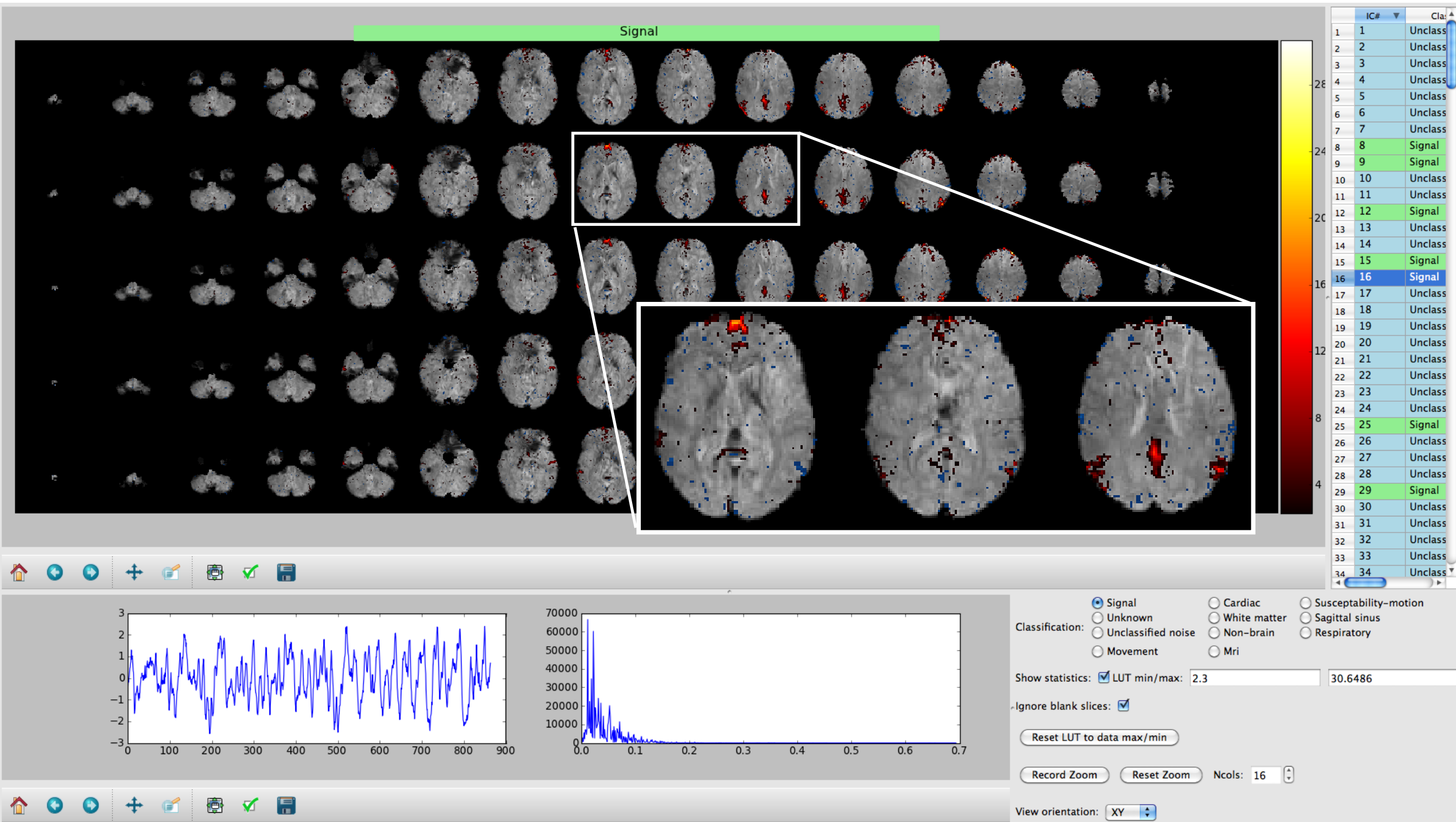
Griffanti NeuroImage 2014

- Preprocessing: head motion correction and drift removal
- FSL's ICA with automatic dimensionality estimation
- FIX
 - classify each ICA component (good v bad)
 - Regress bad ICA timecourses & 24 motion parameters out of data
- FIX component classification accuracy:
 - On good multiband data (eg HCP): 99.5%
 - On “standard” EPI: > 95% TPR, 85% TNR

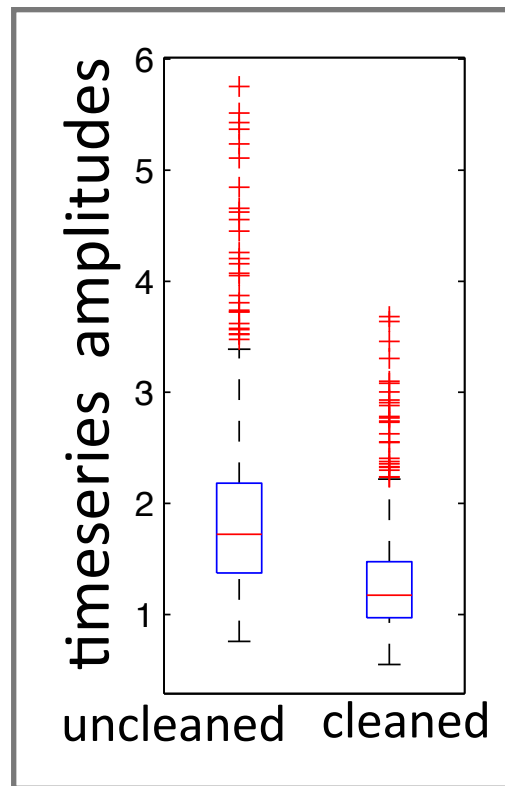
FIX: example artefact component



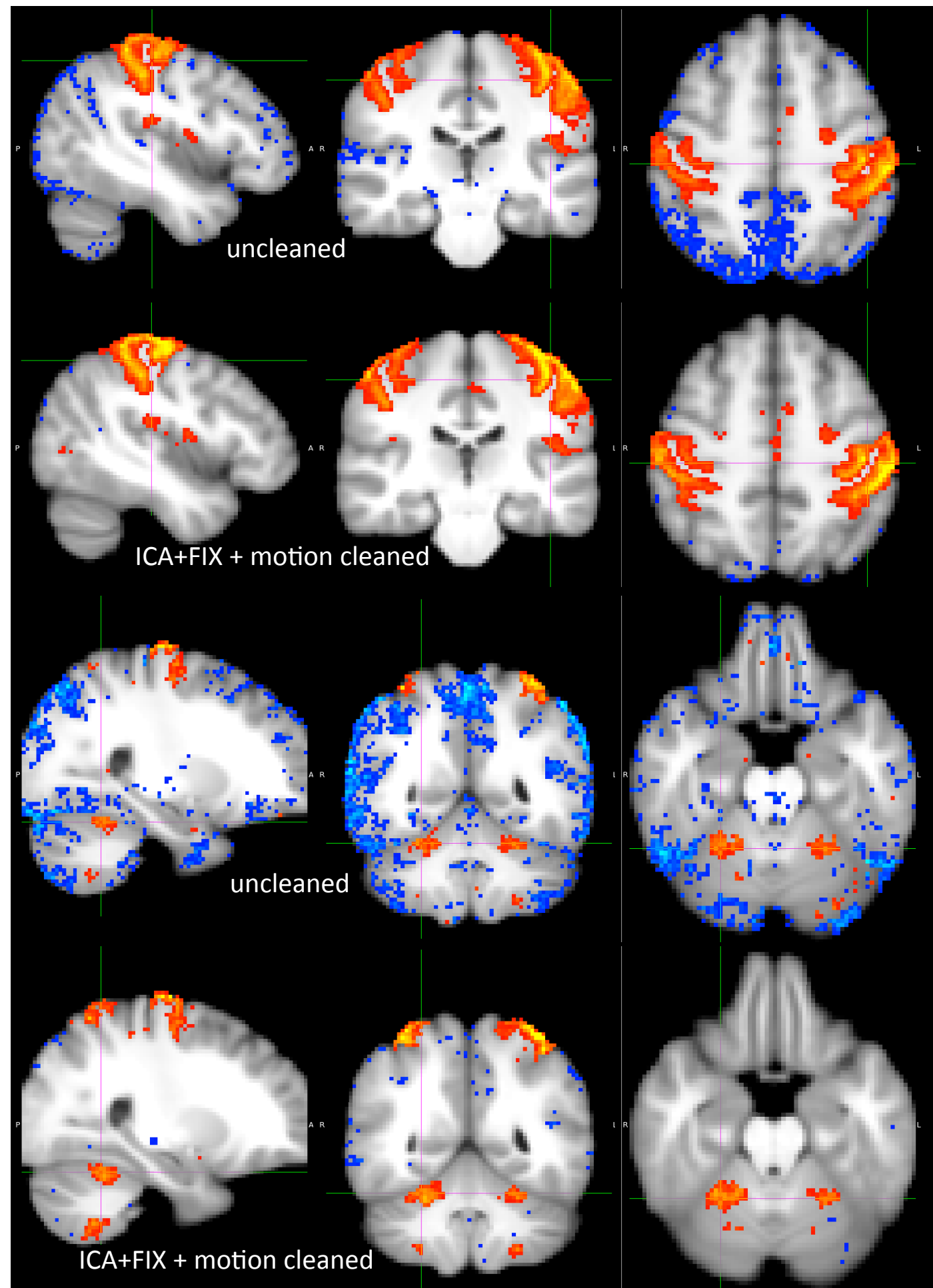
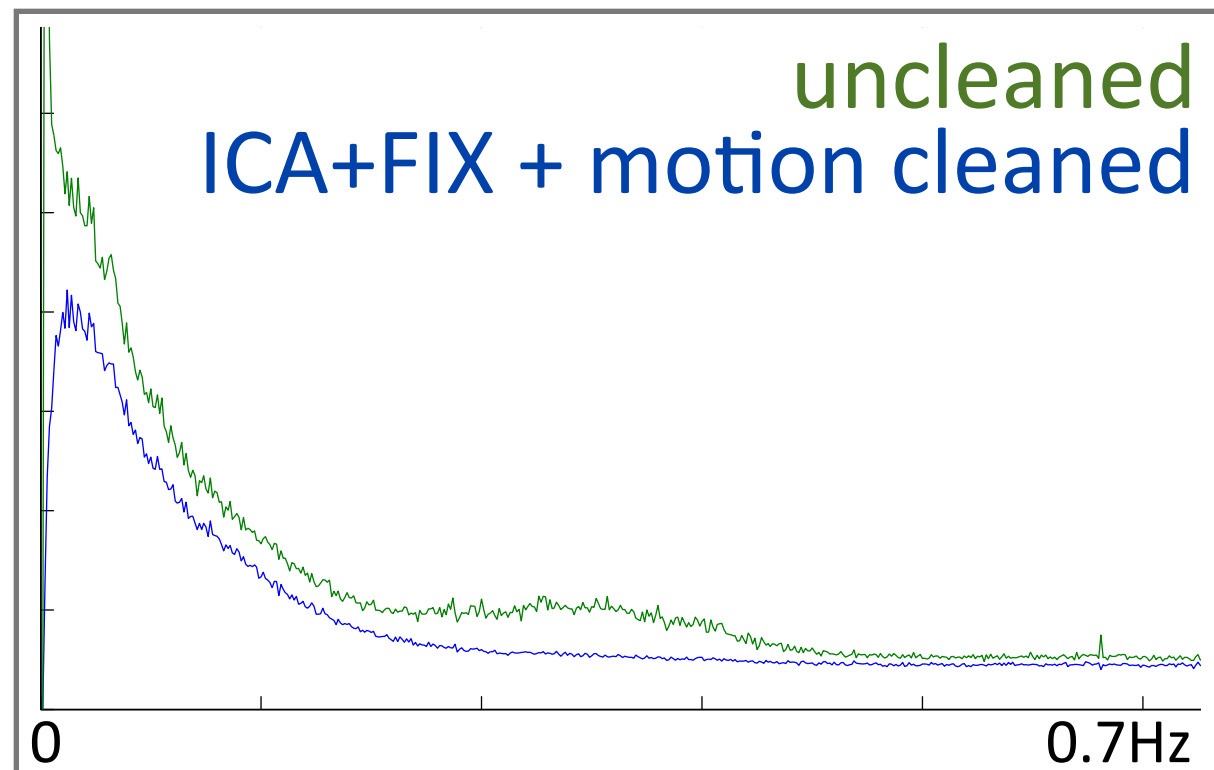
FIX: example good component



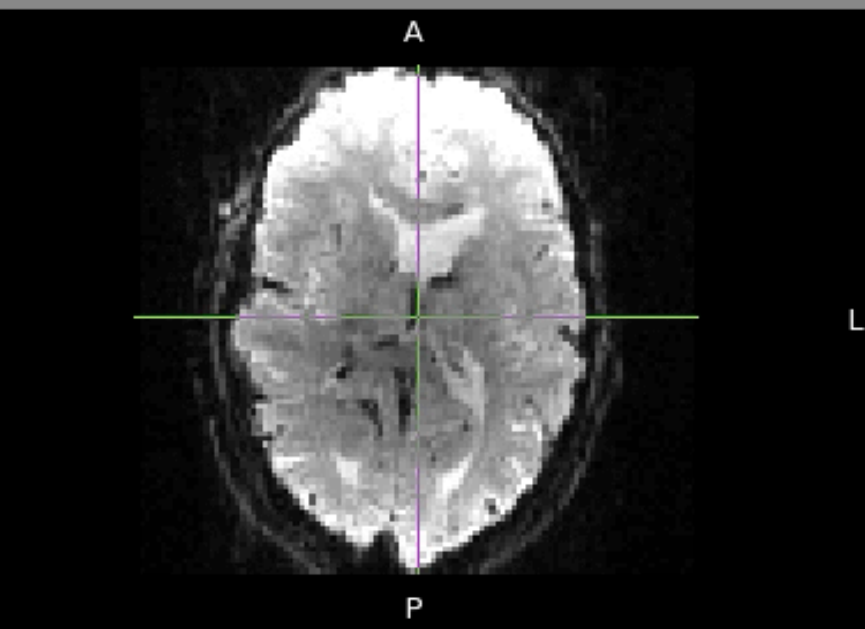
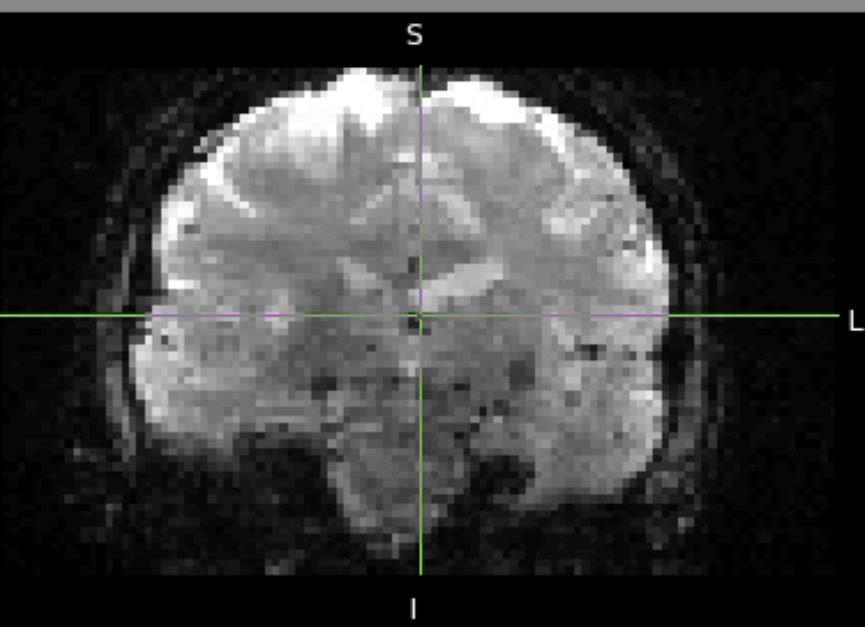
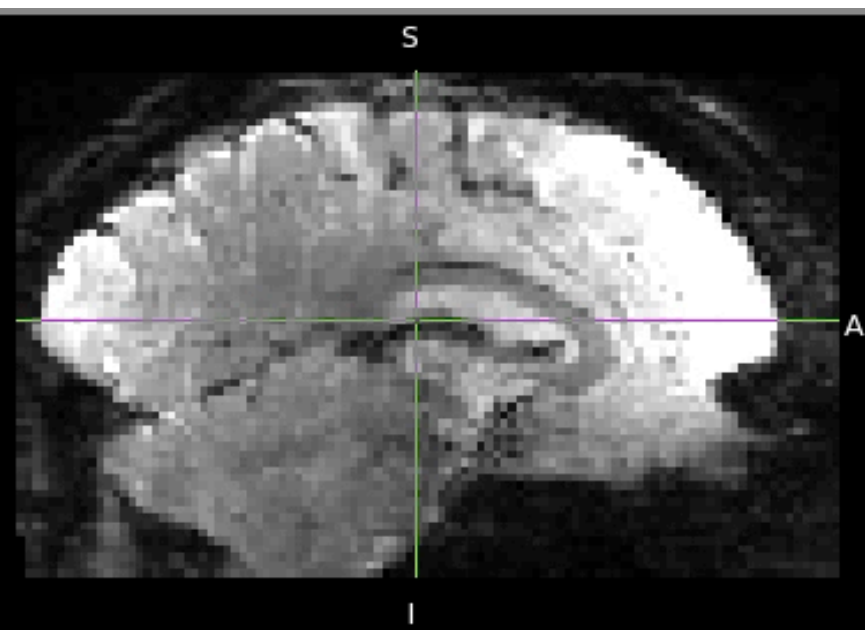
Effect of ICA+FIX cleaning



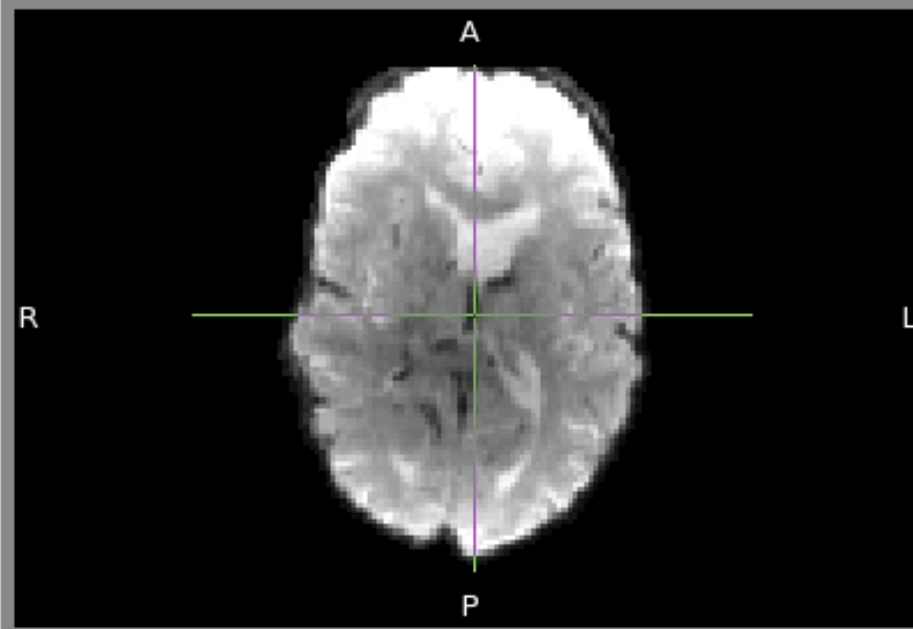
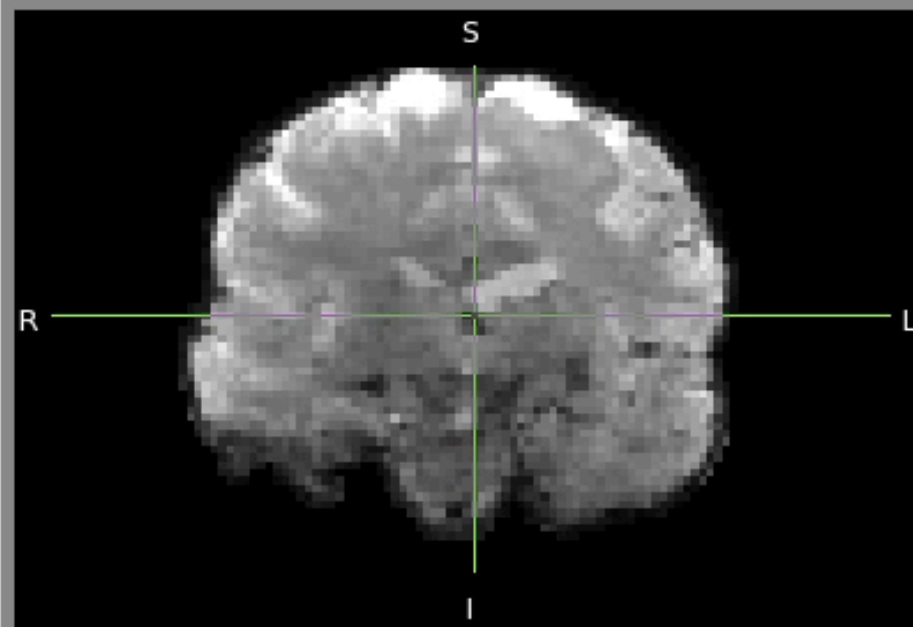
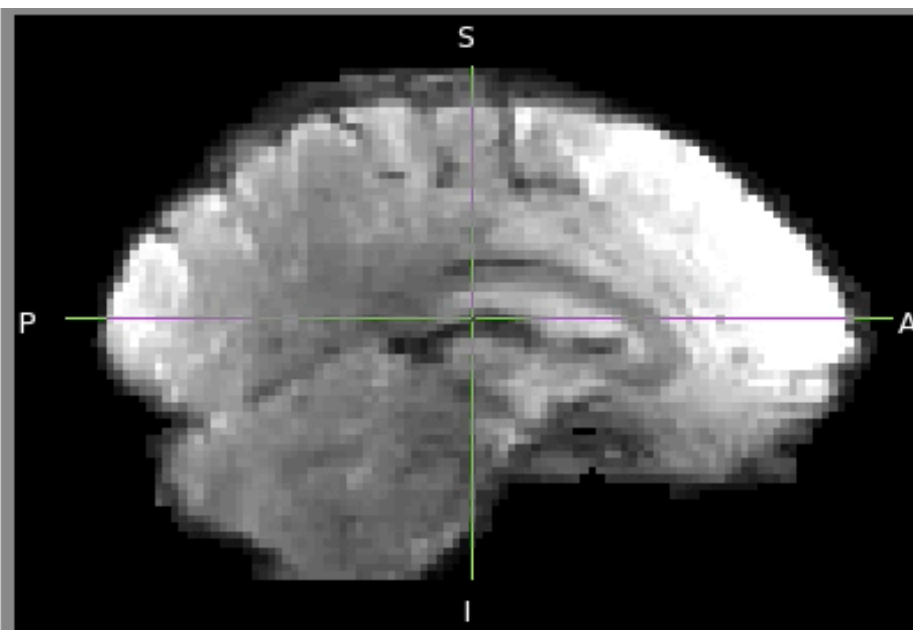
temporal power spectra



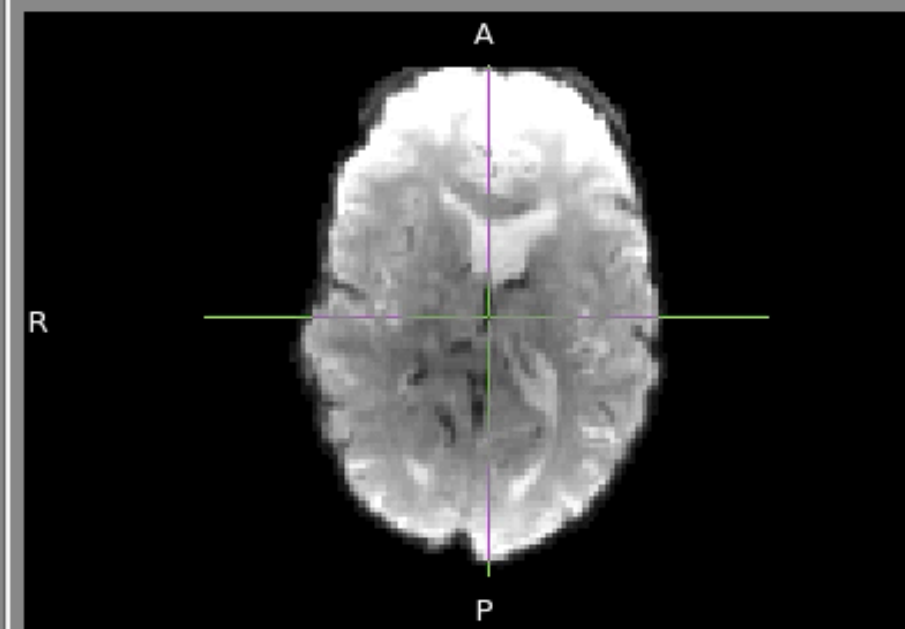
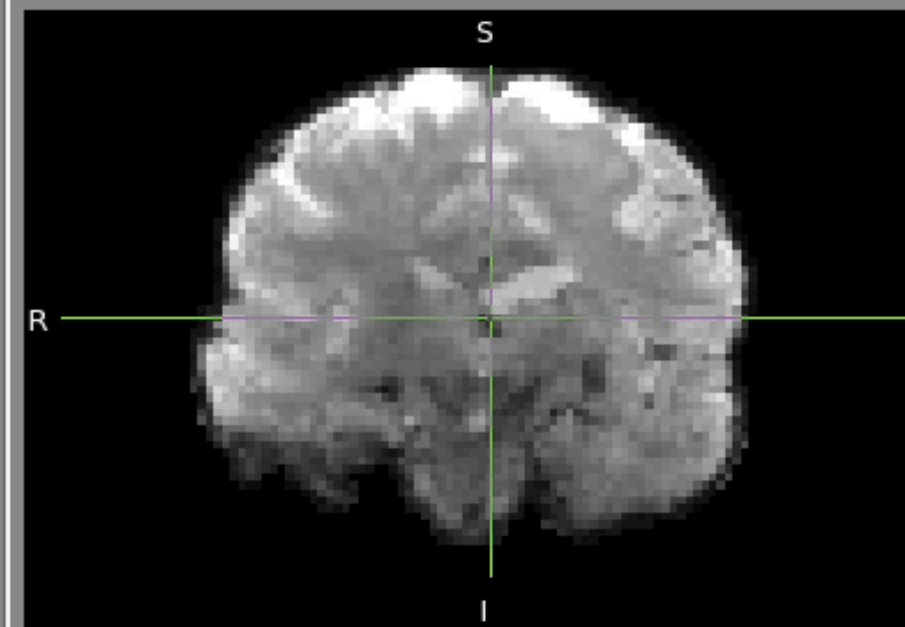
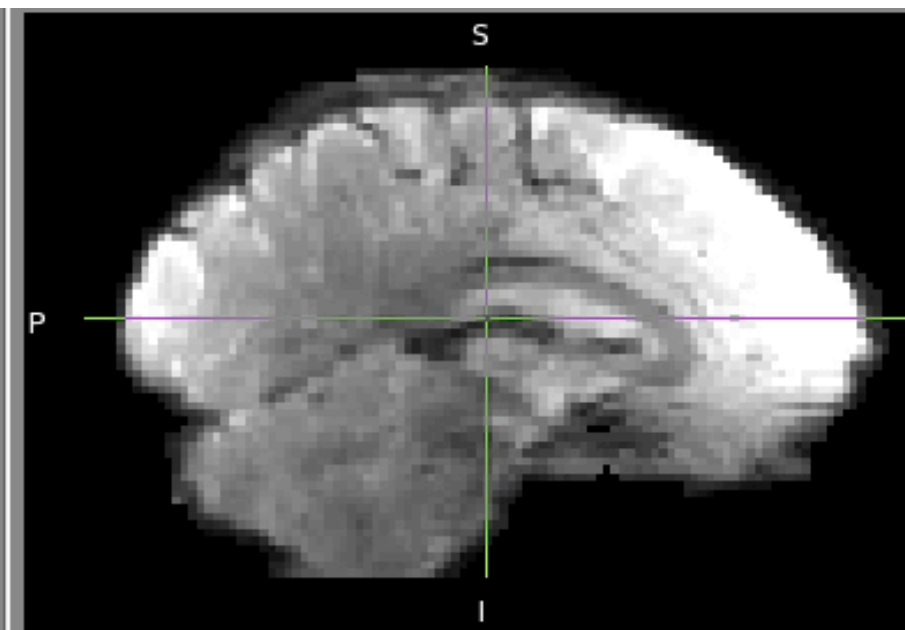
raw data (multiband 6) + preprocessing



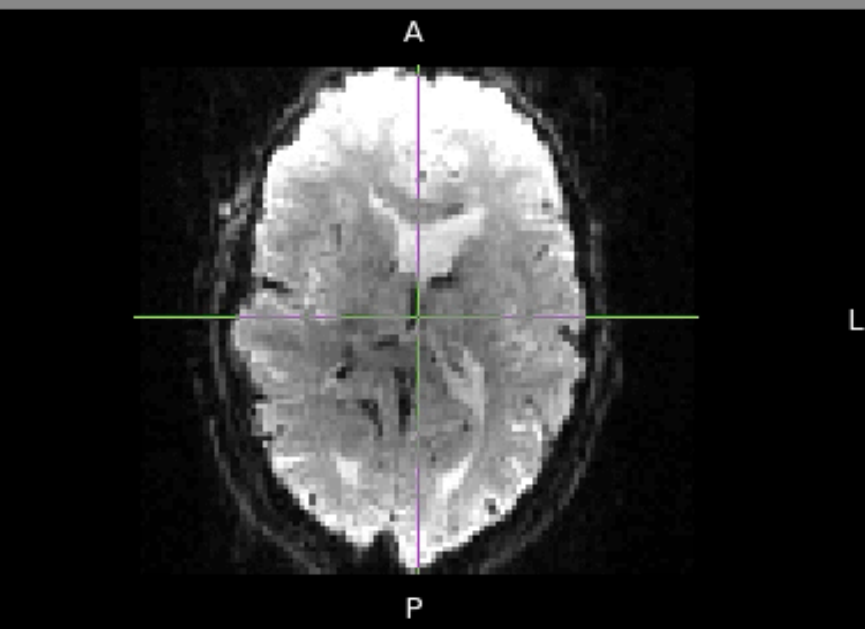
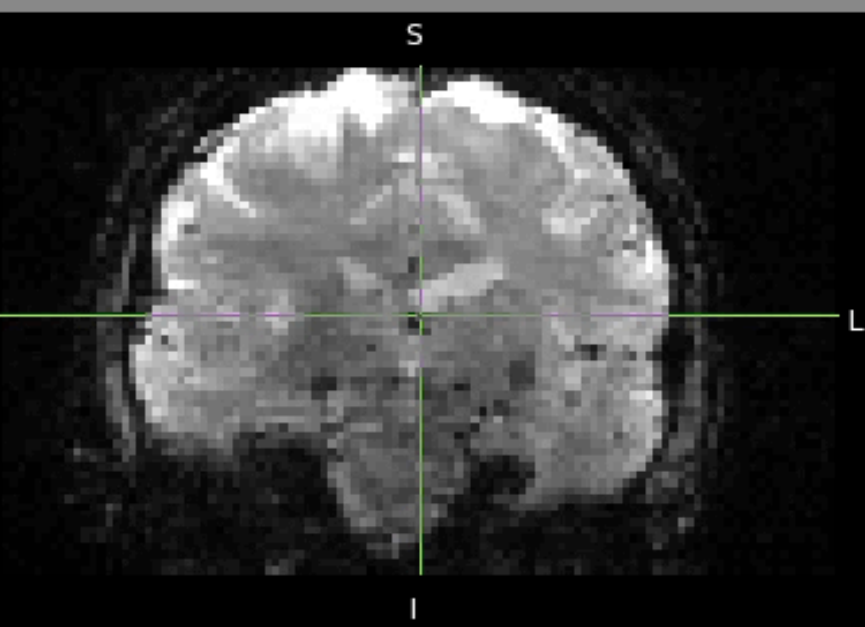
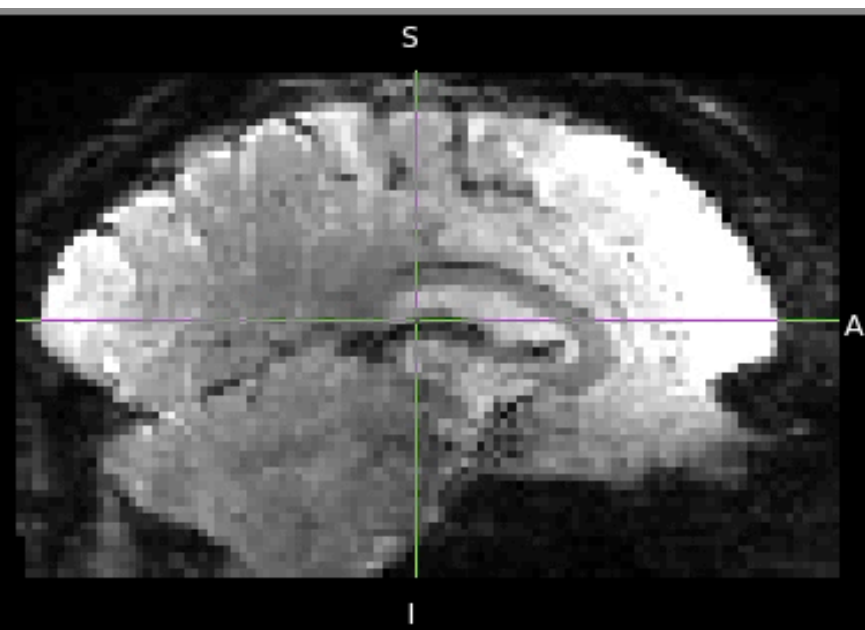
+ preprocessing



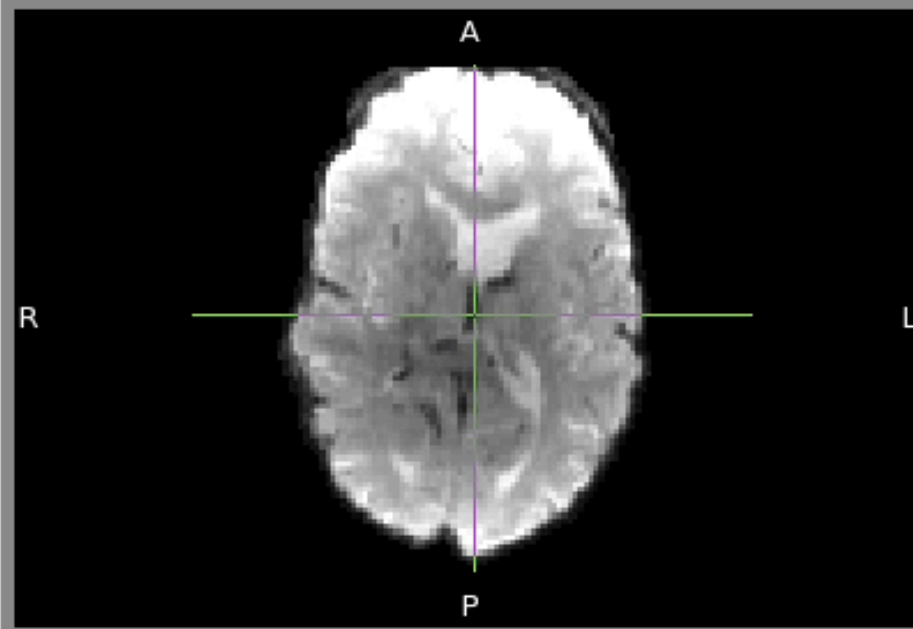
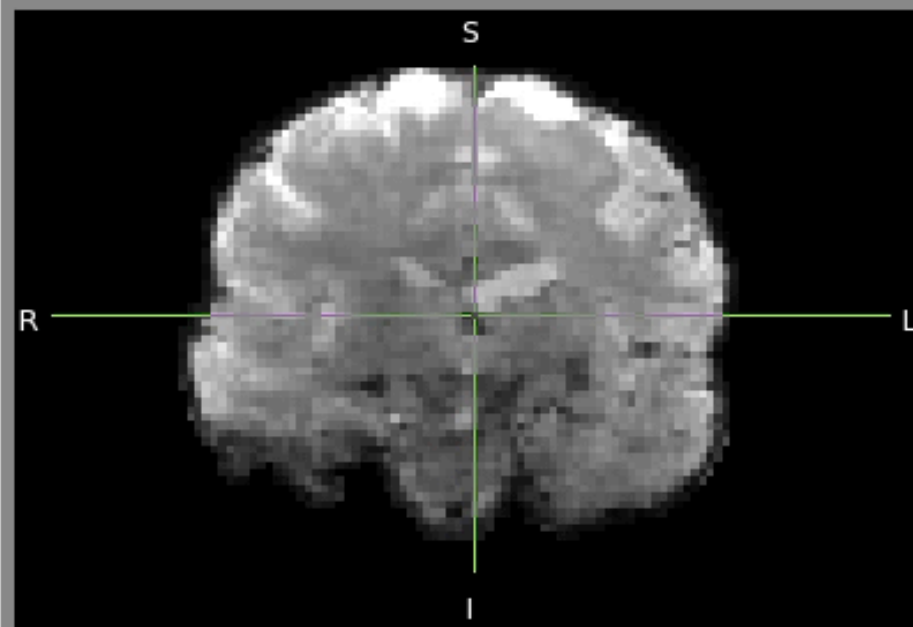
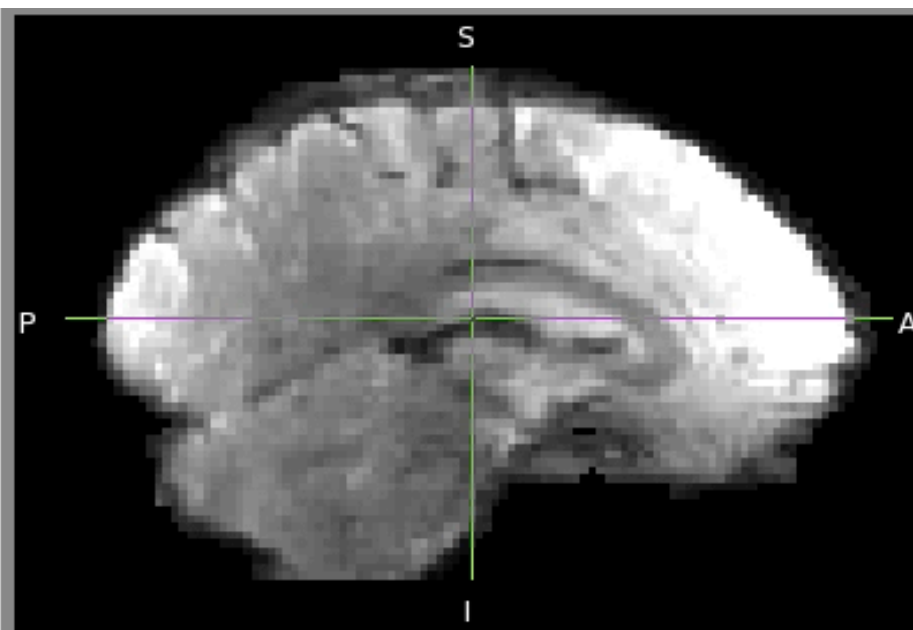
+ ICA+FIX



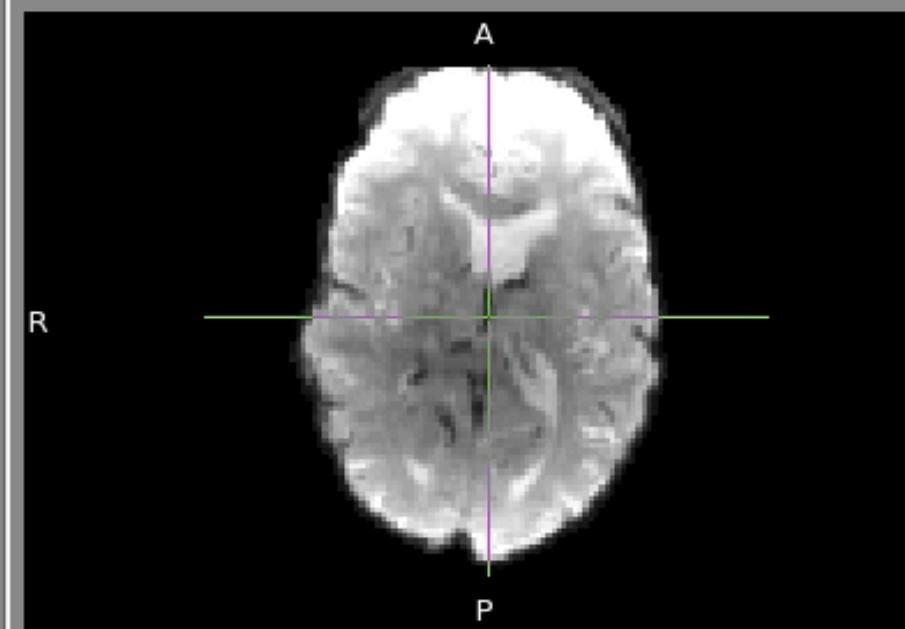
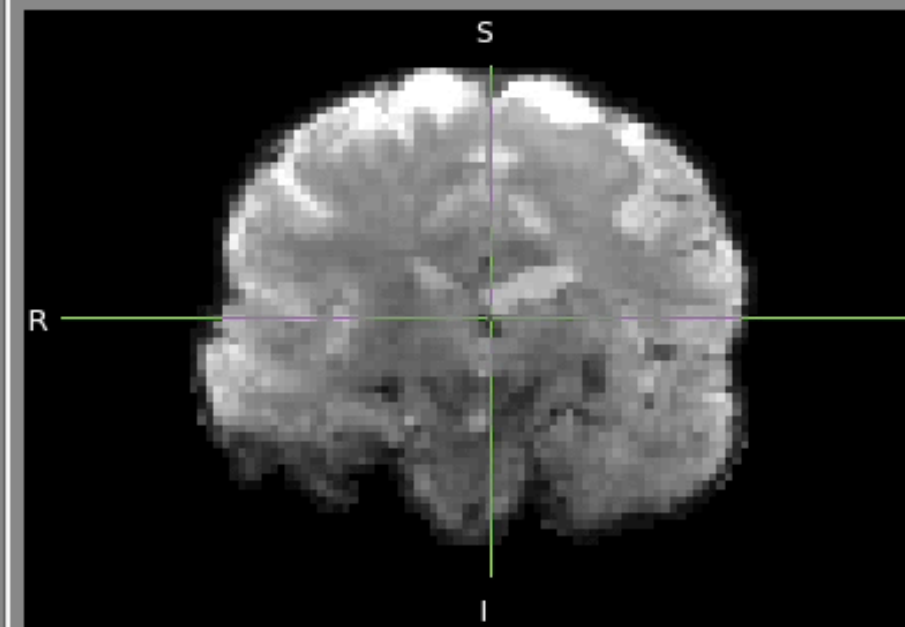
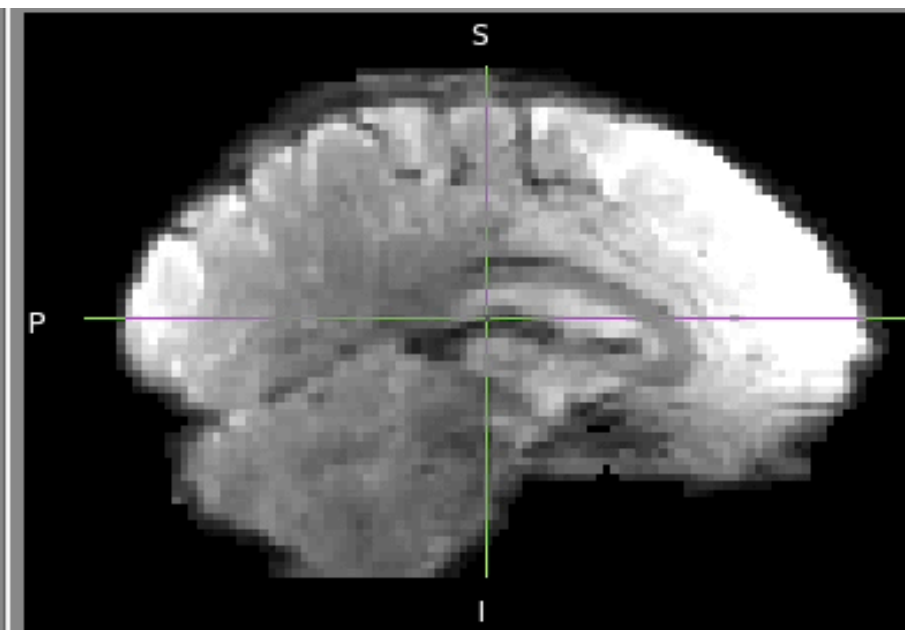
raw data (multiband 6) + preprocessing



+ preprocessing



+ ICA+FIX



Group-level rfMRI analysis

Group Analysis - Seed-Based

- One seed map per subject
- Simple random-effects cross-subject / cross-group analyses using parametric maps from individual subject seedings. Just like task-FMRI GLM cross-subject modelling
- Easy to interpret, and no problems of “correspondence” (do the maps “mean” the same thing in all subjects?) as long as no registration confounds

Group Analysis - ICA

- For any RSN of interest, take each subject's map corresponding to that RSN, somehow
- Simple random-effects cross-subject / cross-group analyses using RSN maps from individual subject seedings.
Just like with seed-based

ICA-based methodology for multi-subject RSN analysis

ICA-based methodology for multi-subject RSN analysis

- Why not just run ICA on each subject separately?
- Correspondence problem (of RSNs across subjects)
- Different splittings *sometimes* caused by small changes in the data (naughty ICA!)

ICA-based methodology for multi-subject RSN analysis

- Why not just run ICA on each subject separately?
 - Correspondence problem (of RSNs across subjects)
 - Different splittings *sometimes* caused by small changes in the data (naughty ICA!)
- Instead - start with a “group-average” ICA
 - But then need to relate group maps back to the individual subjects
 - (*Although* - this approach is less good than single-subject ICA at removing/ignoring session-specific noise)

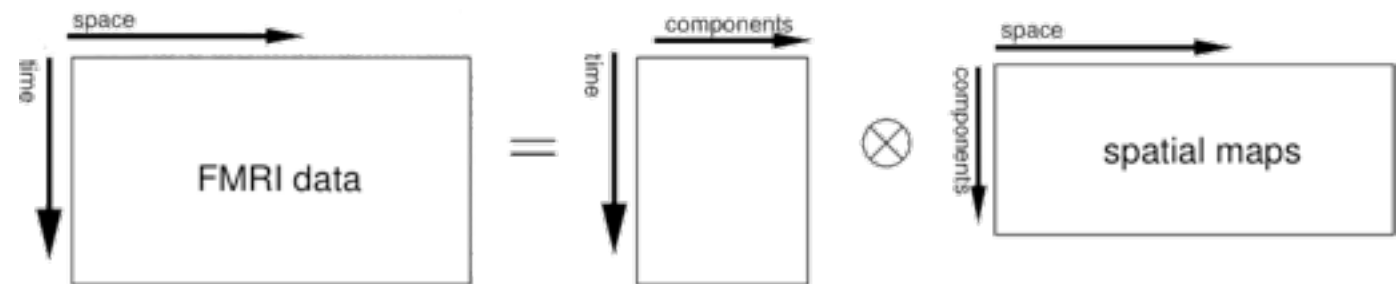
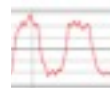
ICA models for RSN analysis

Single-Session ICA

each ICA component comprises:



spatial map & timecourse



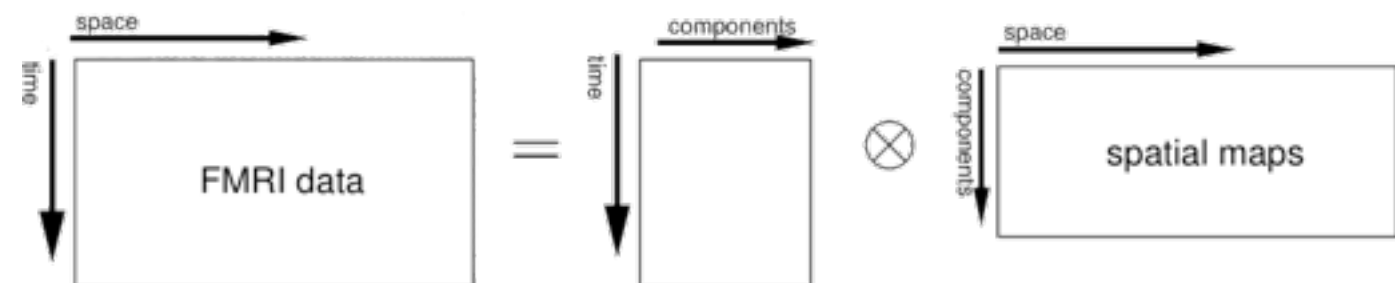
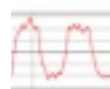
ICA models for RSN analysis

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each ICA component comprises:



spatial map & timecourse



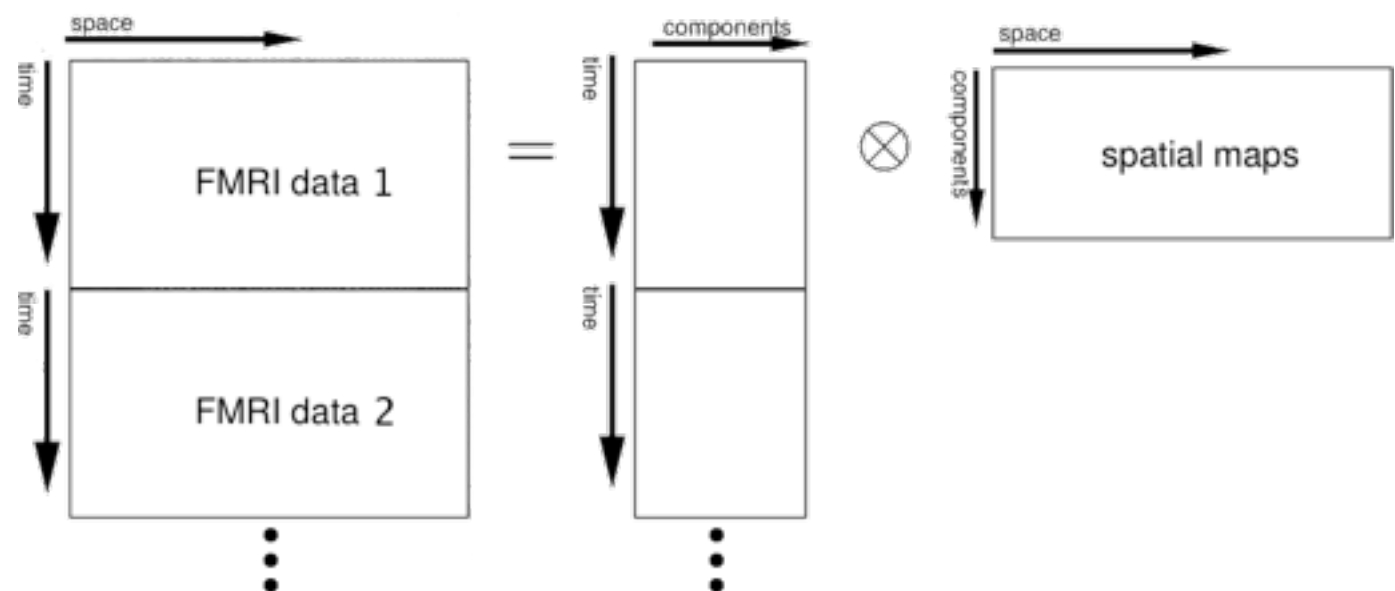
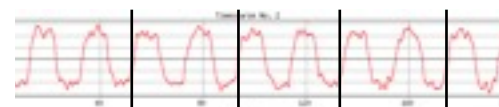
Multi-Session or Multi-Subject ICA: Concatenation approach

each ICA component comprises:



spatial map & timecourse

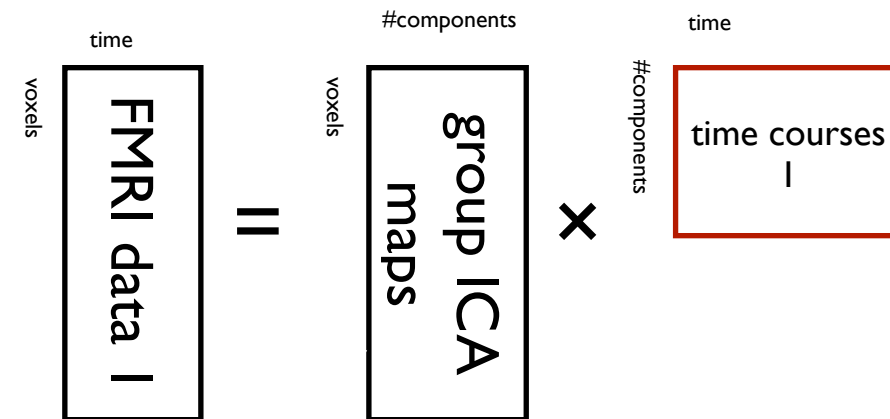
(that can be split up into subject-specific
chunks)



dual regression

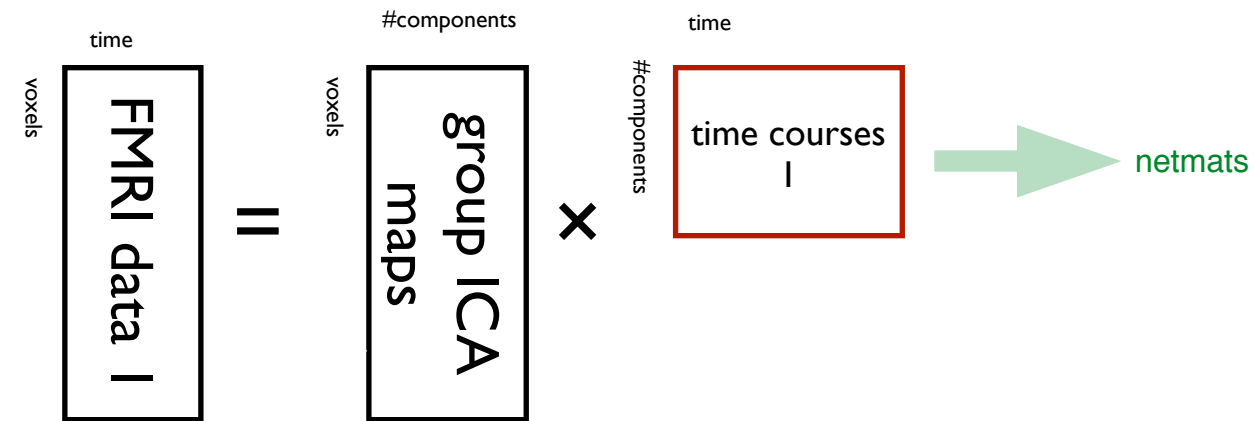
dual regression

- **dr_stage I_subject[#SUB].txt** - the *timeseries* outputs of stage I of the dual-regression.



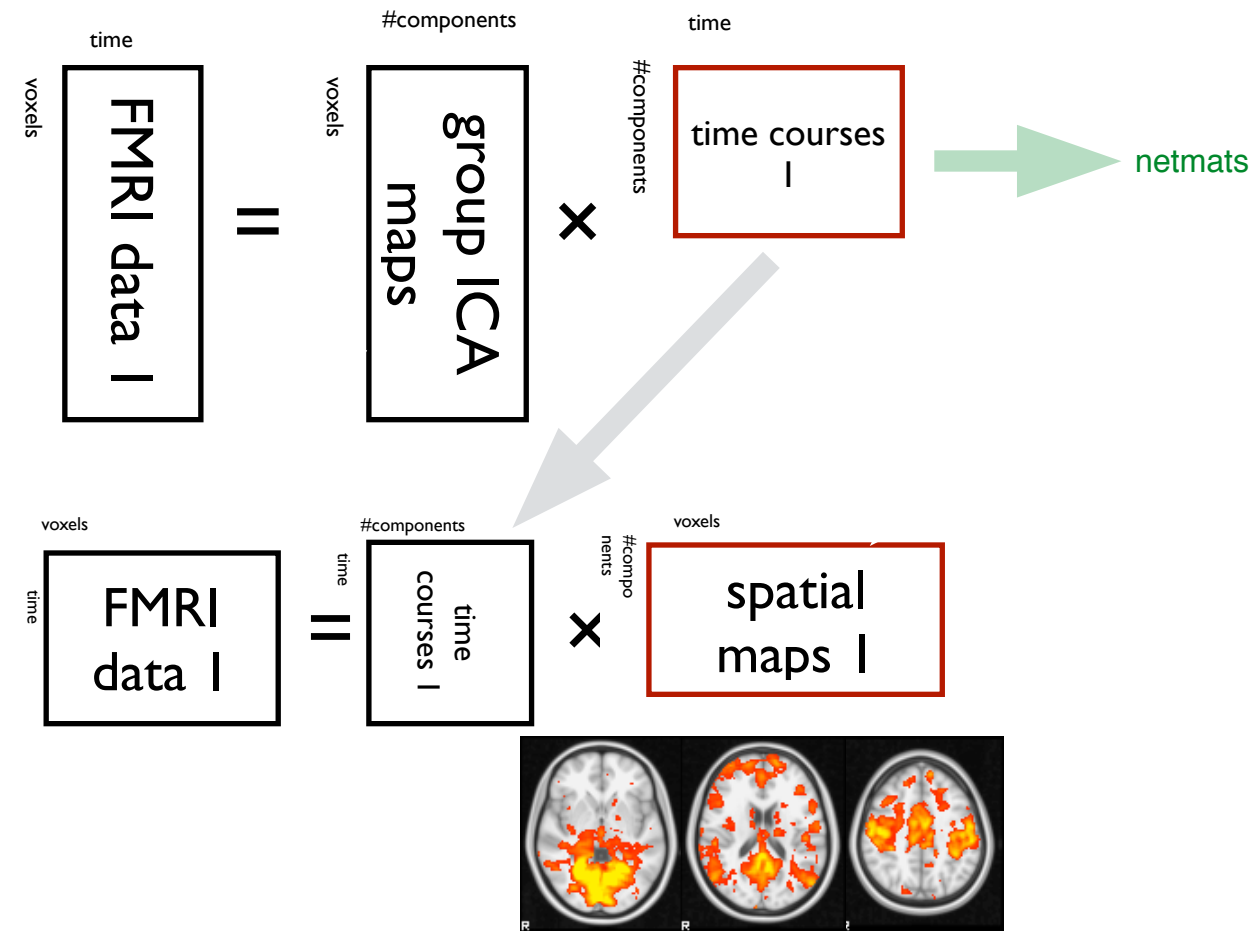
dual regression

- **dr_stage I_subject[#SUB].txt** - the *timeseries* outputs of stage I of the dual-regression.



dual regression

- **dr_stage1_subject[#SUB].txt** - the *timeseries* outputs of stage 1 of the dual-regression.
- **dr_stage2_subject[#SUB].nii.gz** - the *spatial maps* outputs of stage 2 of the dual-regression.

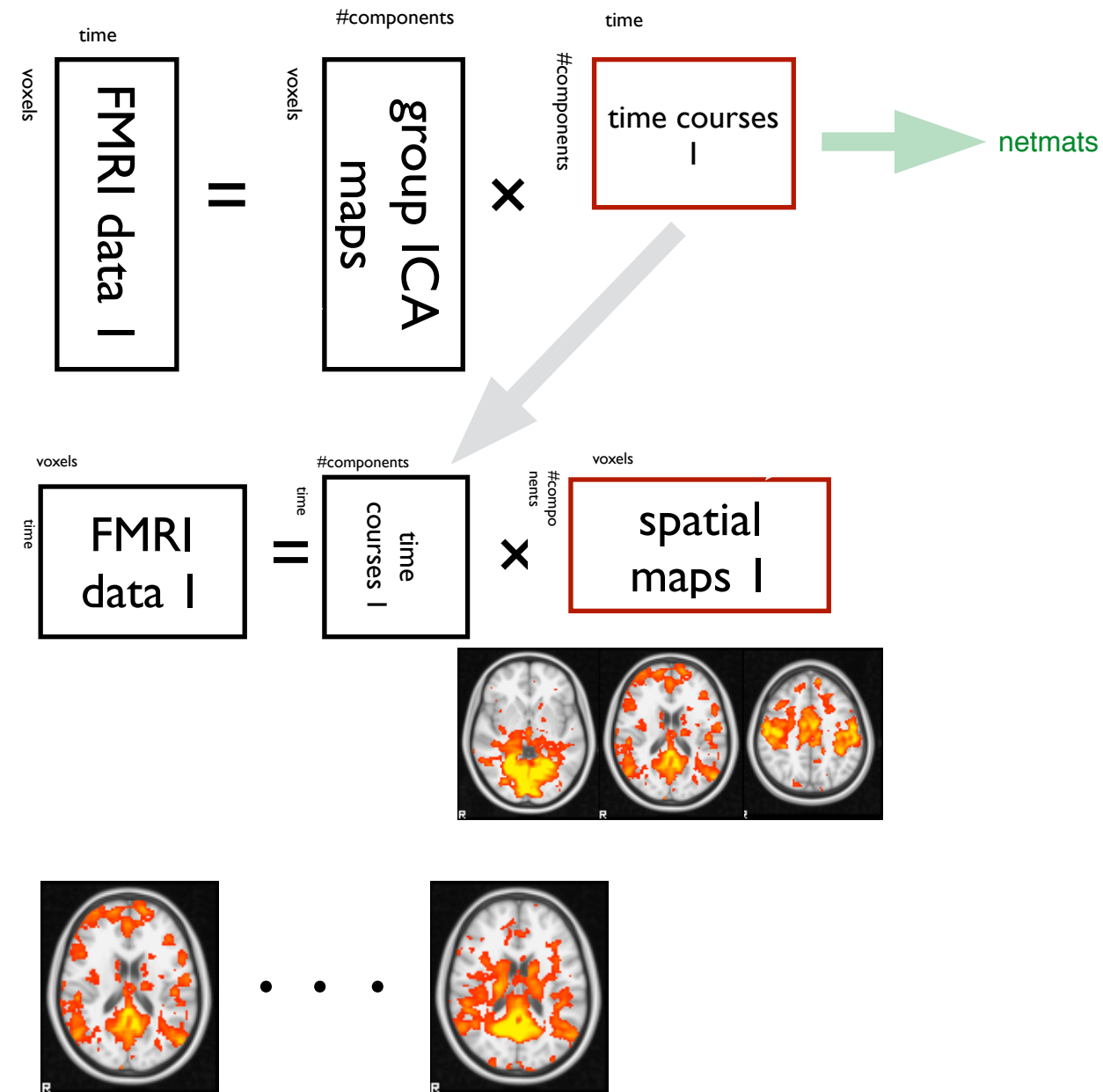


dual regression

- **dr_stage1_subject[#SUB].txt** - the *timeseries* outputs of stage 1 of the dual-regression.

- **dr_stage2_subject[#SUB].nii.gz** - the *spatial maps* outputs of stage 2 of the dual-regression.

- **dr_stage2_ic[#ICA].nii.gz** - the re-organised parameter estimate images



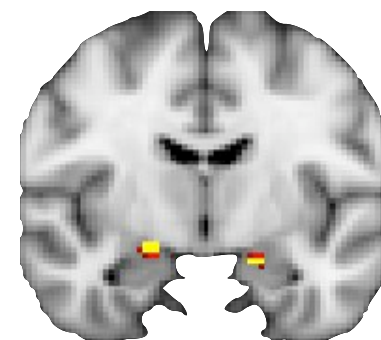
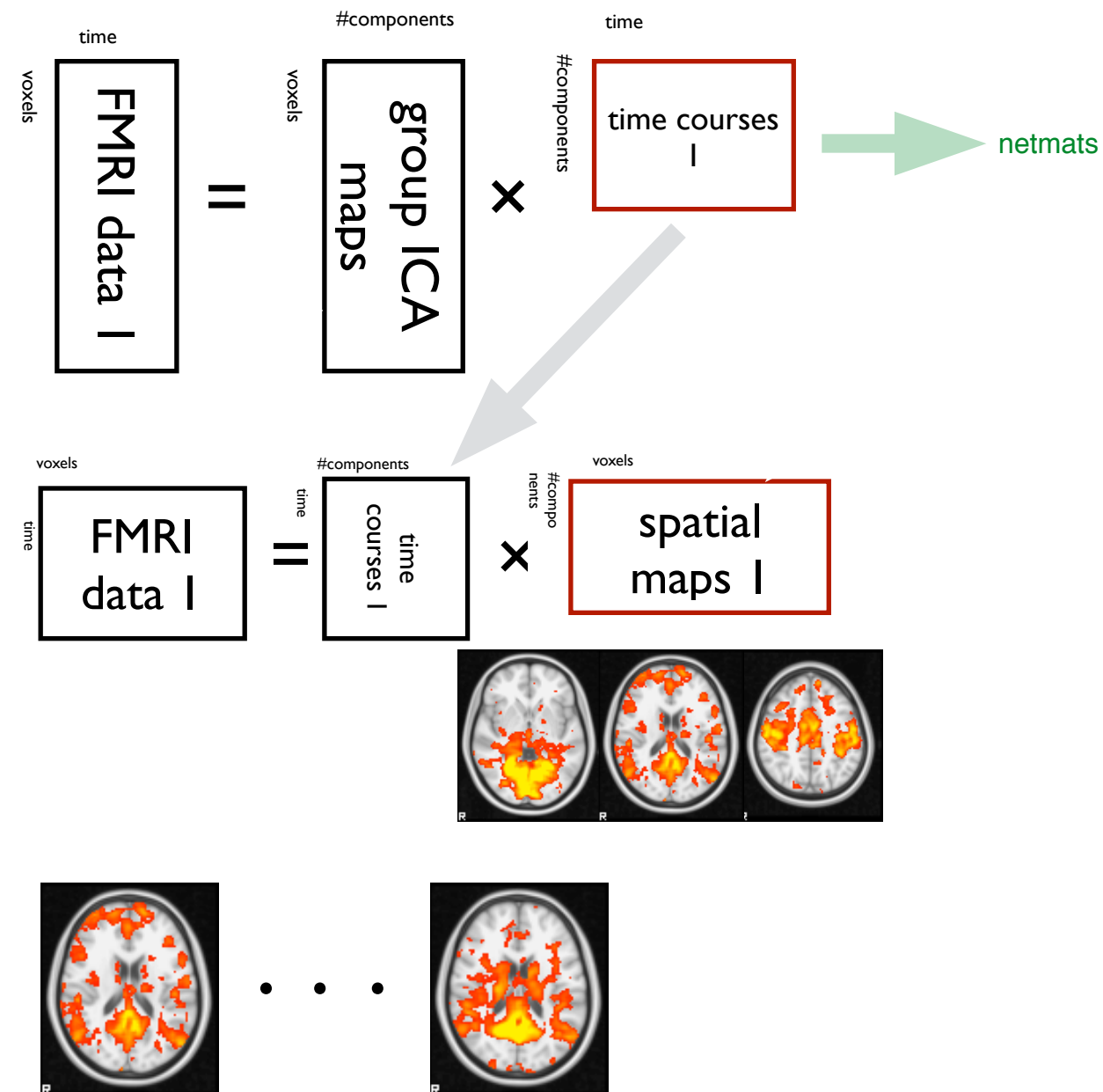
dual regression

- **dr_stage1_subject[#SUB].txt** - the *timeseries* outputs of stage 1 of the dual-regression.

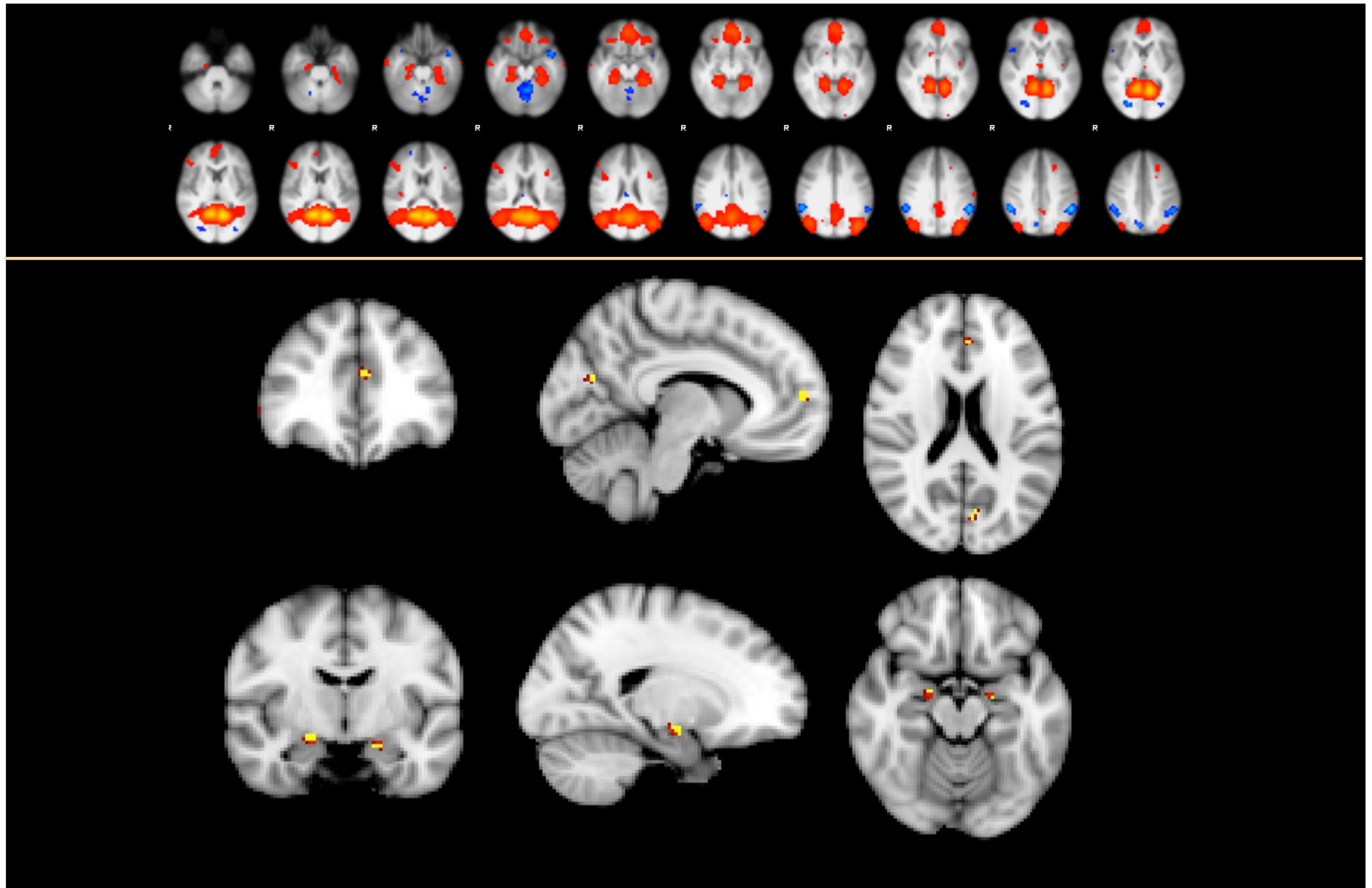
- **dr_stage2_subject[#SUB].nii.gz** - the *spatial maps* outputs of stage 2 of the dual-regression.

- **dr_stage2_ic[#ICA].nii.gz** - the re-organised parameter estimate images

- **dr_stage3_ic[#ICA]_tstat[#CON].nii.gz** - the output from randomise
(corrected for mc across voxels but not across #components!!)



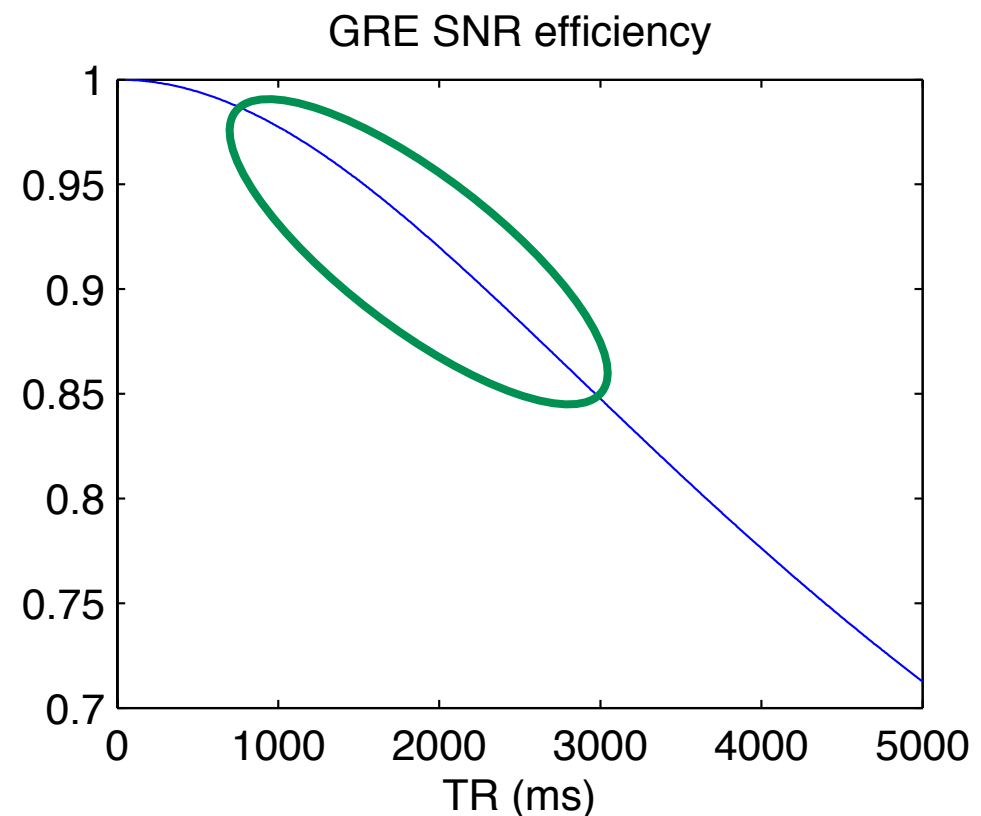
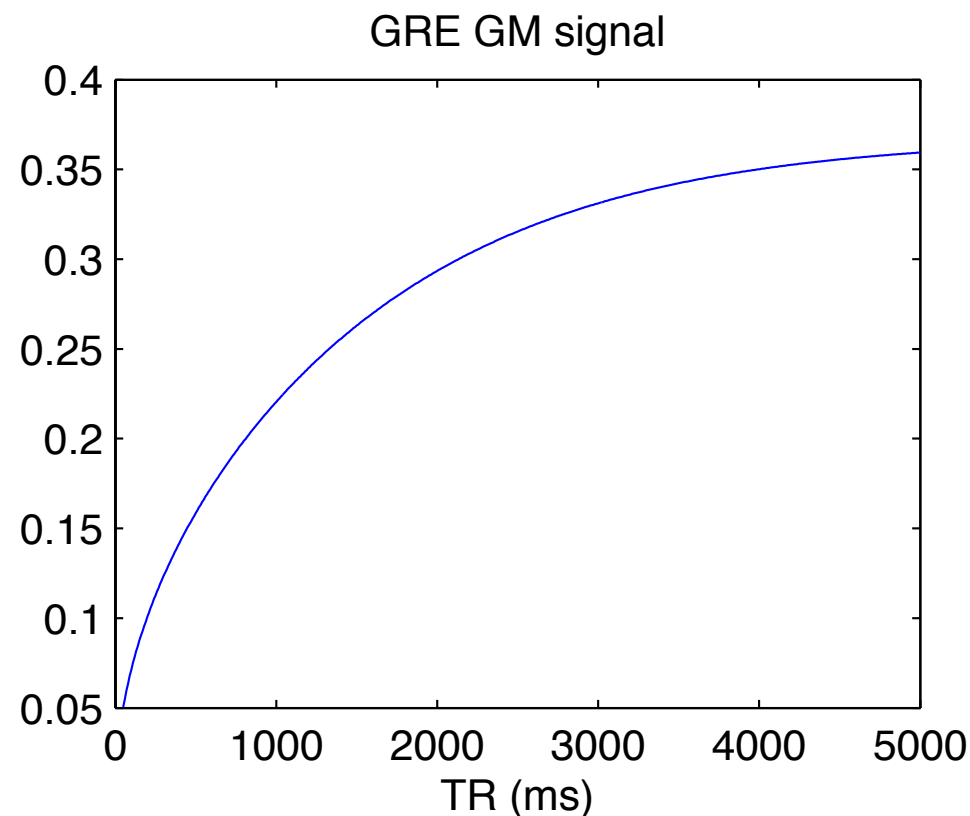
Altered functional connectivity in young, healthy carriers of APOE- ϵ 4

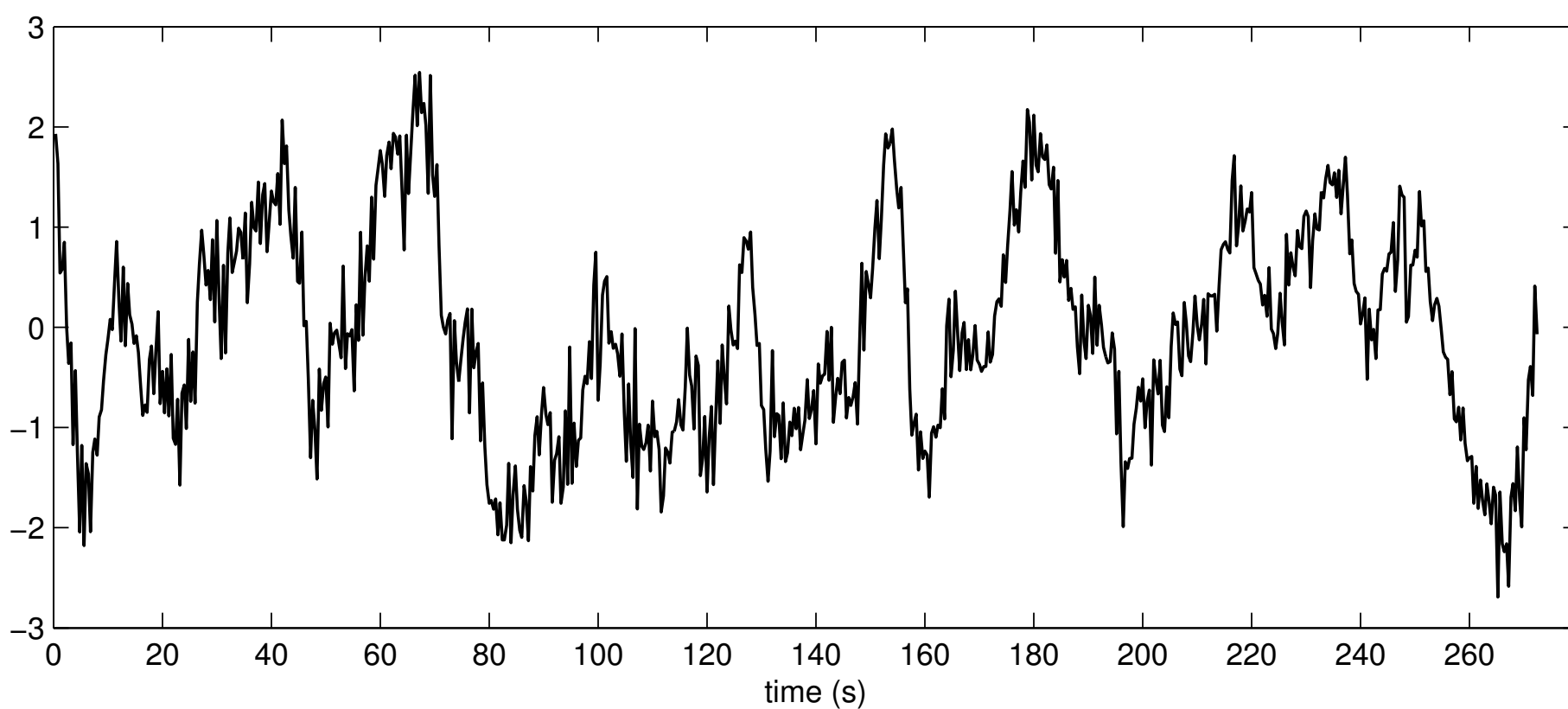
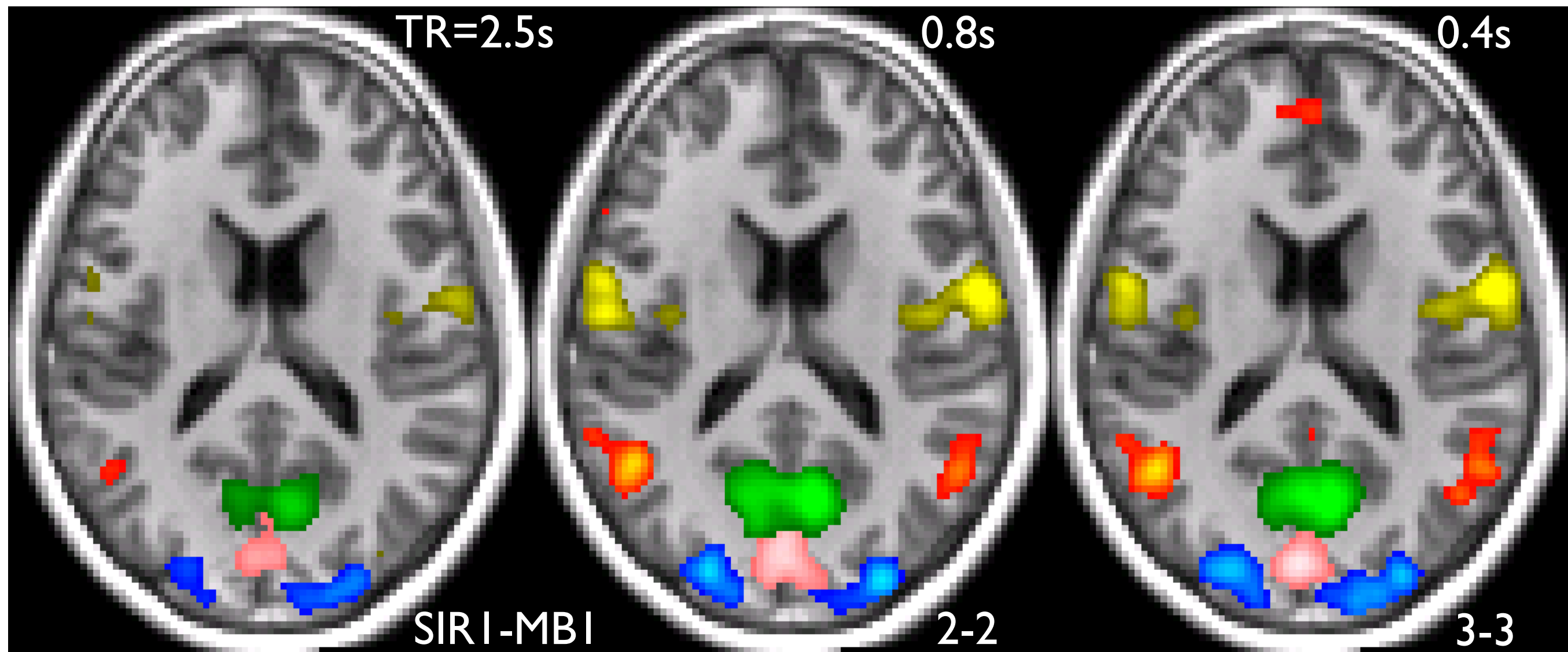


НСР

Signal & Noise Considerations

- Main SNR effect (when reducing TR) is *signal loss* due to reduced T_1 -relaxation period
- This loss almost balanced by the \sqrt{N} increase in effective SNR





- Increased DoF and temporal sampling
- Non-Gaussianity
- Non-stationarity
- Interesting temporal dynamics

HCP rfMRI pre-processing summary

- 4D rfMRI data from *spatial* (“minimal”) *pre-processing*, in both volumetric and grayordinate forms
- Weak highpass temporal filtering (>2000s FWHM) applied to both, giving slow drift removal
- MELODIC ICA is applied to volumetric data; artefact components are identified using FIX
- Artefact and motion-related timecourses are regressed out of both volumetric and grayordinate data
- Ongoing investigations into also possibly applying:
 - further motion cleanup / scrubbing
 - further removal of physiological confounds based on physiological monitoring data
 - removal of globally-related signals.

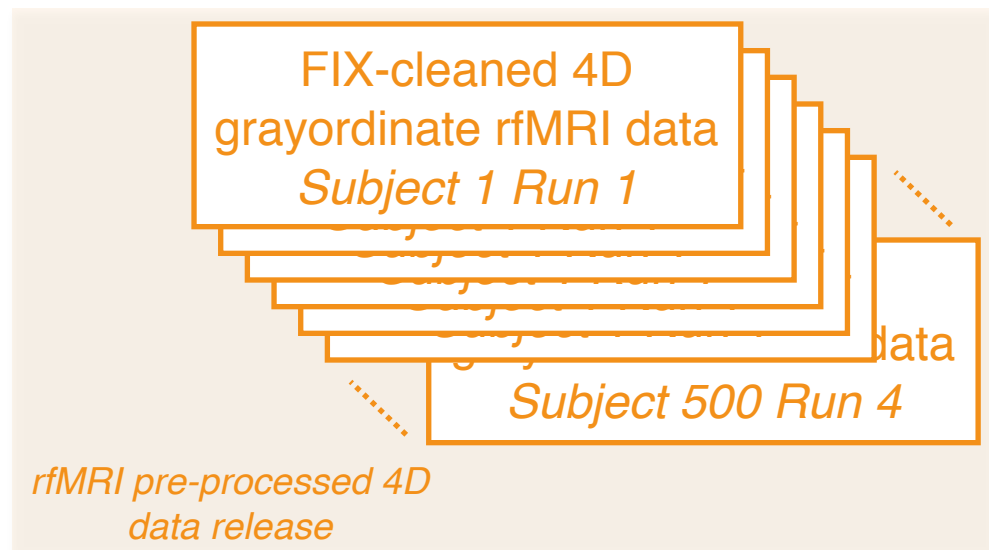
HCP rfMRI data

processing flowchart

and data release info

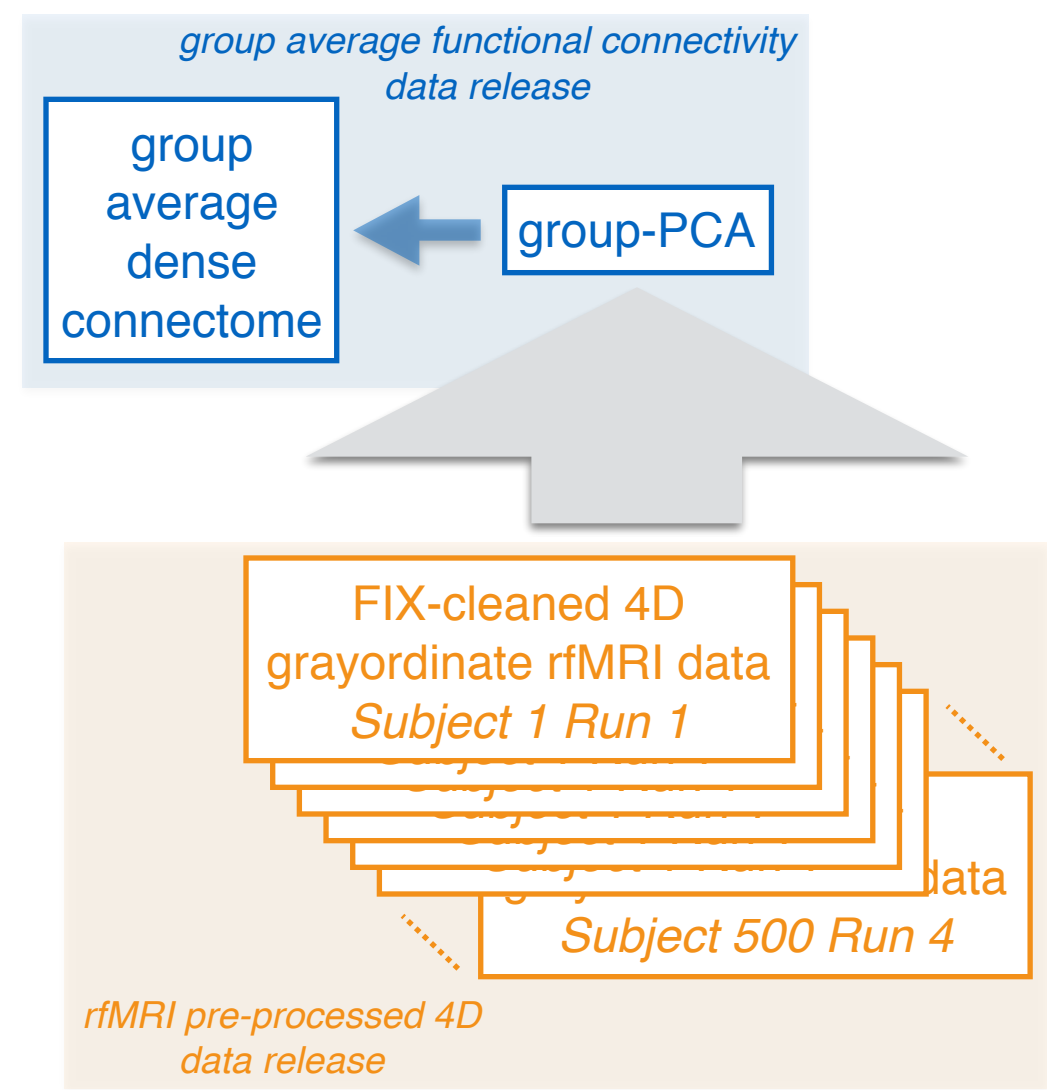
HCP rfMRI data

processing flowchart
and data release info



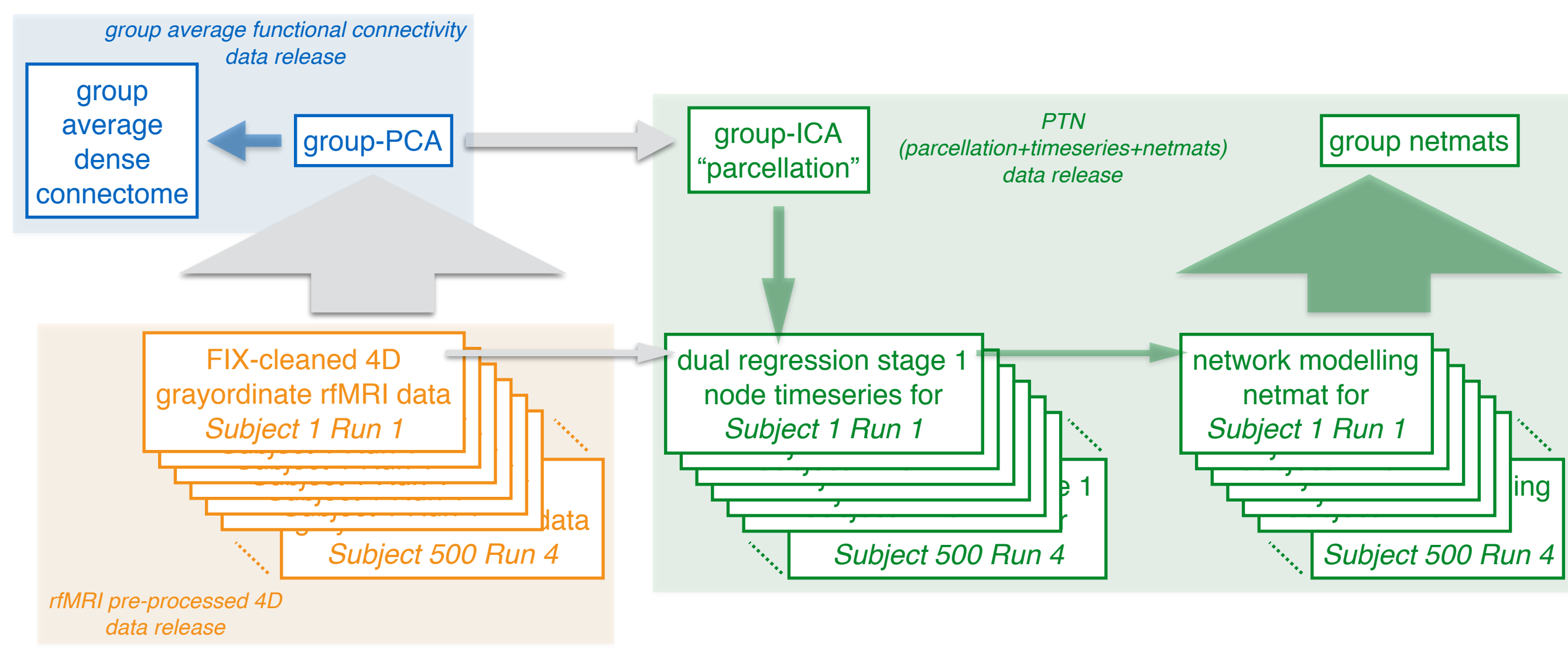
HCP rfMRI data

processing flowchart
and data release info



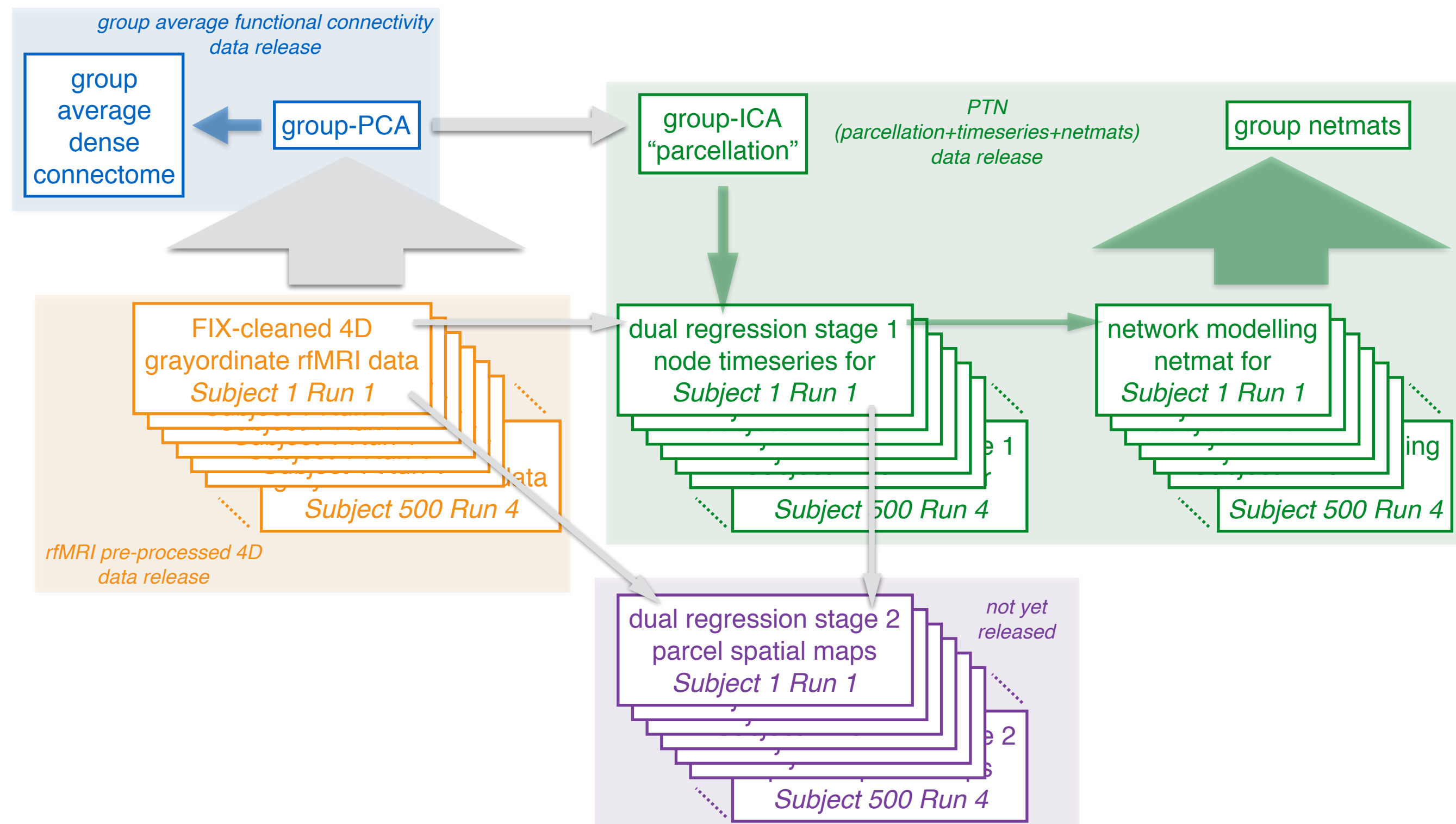
HCP rfMRI data

processing flowchart
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